

White matter fibre density in the brain’s inhibitory control network is associated with falling in older adults

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April 23, 2024

Abstract

Recent research has indicated that the relationship between age-related cognitive decline and falling may be mediated by the individual’s capacity to quickly cancel or inhibit a motor response. This longitudinal investigation demonstrates that higher white matter fibre density in the motor inhibition network paired with low physical activity was associated with falling in elderly participants. We measured the density of white matter fibre tracts connecting key nodes in the inhibitory control network in a large sample (n=414) of older adults. We modelled their self-reported frequency of falling over a four year period with white matter fibre density in pathways corresponding to the direct and hyperdirect cortical-subcortical loops implicated in the inhibitory control network. Only connectivity between right Inferior Frontal Gyrus and right Subthalamic Nucleus was associated with falling as measured cross-sectionally. The connectivity was not, however, predictive of future falling when measured two and four years later. Higher white matter fibre density was associated with falling, but only in combination with low levels of physical activity. No such relationship existed for selected control brain regions that are not implicated in the inhibitory control network. The direction of this effect was counterintuitive and warrants further longitudinal investigation into whether white matter fibre density changes over time in a manner correlated with falling, and mediated by physical activity.

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19 Acknowledgements

20 KR would like to acknowledge funding from the Health Research Board, Ireland grant
21 number EIA-2019-003. CS would like to thank Daniel Araya R. for helpful comments and
22 discussions relating to this work.

23

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27 **Abstract**

28 Recent research has indicated that the relationship between age-related cognitive decline and
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30 response. This longitudinal investigation demonstrates that higher white matter fibre density in
31 the motor inhibition network paired with low physical activity was associated with falling in
32 elderly participants. We measured the density of white matter fibre tracts connecting key nodes
33 in the inhibitory control network in a large sample (n=414) of older adults. We modelled their
34 self-reported frequency of falling over a four year period with white matter fibre density in
35 pathways corresponding to the direct and hyperdirect cortical-subcortical loops implicated in
36 the inhibitory control network. Only connectivity between right Inferior Frontal Gyrus and
37 right Subthalamic Nucleus was associated with falling as measured cross-sectionally. The
38 connectivity was not, however, predictive of future falling when measured two and four years
39 later. Higher white matter fibre density was associated with falling, but only in combination
40 with low levels of physical activity. No such relationship existed for selected control brain
41 regions that are not implicated in the inhibitory control network. The direction of this effect
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43 fibre density changes over time in a manner correlated with falling, and mediated by physical
44 activity.

45

46 Keywords: Ageing, Falling, inhibitory control, DTI, white matter, physical activity

48 It is now well established that as higher order cognitive abilities decline with ageing, the
49 incidence of falling increases proportionally (Amboni et al., 2013; Ambrose et al., 2013;
50 Herman et al., 2010; Kearney et al., 2013; Li et al., 2018; Mirelman et al., 2012; Montero-
51 Odasso et al., 2012; Muir et al., 2012). However, the structural and functional neural
52 mechanisms underlying this relationship remain undefined. In-depth behavioural testing has
53 revealed that inhibitory control, a specific facet of executive function, is especially predictive
54 of falling. In a longitudinal study, Mirelman et al., (2012) demonstrated that an individual's
55 capacity for effective inhibitory control measured by computerised tests was predictive of fall
56 prevalence in the subsequent 5 year period. This suggests that response inhibition, the ability
57 to suppress highly automatic action in situations where such instinctive action is unwarranted
58 (Fuster, 2008), may play a significant role in fall prevention. Furthermore, response inhibition
59 is closely related to cognitive flexibility or the ability to adapt to complex and rapidly changing
60 environments (Diamond, 2013) which correlates with fall prevalence (Kearney et al., 2013;
61 Pieruccini-Faria et al., 2019). While the ability to stop may seem an unusual prerequisite for
62 effective balance control, we often need to rapidly adapt our posture while navigating real-
63 world settings. This entails occasional but appropriate suppression and revision of reflexive
64 movements.

65 Many factors contribute to maintaining postural equilibrium such as strength (Okubo et al.,
66 2022; Pijnappels et al., 2008), sensory acuity (Brown et al., 2015; Reed-Jones et al., 2013),
67 blood pressure regulation (Kenny et al., 2017), and cognitive ability Mirelman et al. (2012),
68 and this makes it difficult to ascribe a particular role to any one culprit leading to a fall. Several
69 studies have attempted to tease out the relative contribution of convergent factors that affect
70 fall risk, including the influence of distinct cognitive abilities. For example, Holtzer et al.
71 (2007) studied if specific cognitive abilities were related to falls in a large sample of community
72 dwelling older adults without cognitive impairment while also accounting for gait
73 abnormalities (another factor related to falls (Tinetti et al., 1988). Among separate cognitive
74 domains of verbal IQ, speed/executive attention, and memory, only speed/executive attention
75 was related to retrospective falls. This suggested that global cognitive ability was not driving
76 this effect (a finding consistent with Mirelman et al. (2012) where Executive Function
77 predicted falls but overall cognitive scores were uninformative). Notably, Holtzer et al. (2007)
78 revealed an effect independent of gait-related issues. More recently, Okubo et al. (2022)
79 measured several standard fall-risk variables such as leg strength, postural sway, simple and

80 choice reaction time, etc., in relation to performance on a laboratory-based perturbation
81 paradigm where participants needed to adapt their gait to prevent a fall and the strongest
82 predictor of balance recovery was performance on a hand-based test (ReacStick) of rapid
83 inhibition accuracy. The aforementioned studies collectively suggest that inhibitory control
84 plays an important role in preventing falls. This seems to be the case even when global
85 cognitive measures fail to correlate with falls, and this role is independent of strength and
86 general processing speed.

87 Beyond correlational data linking cognitive performance with falls, there have been
88 several laboratory-based studies showing empirically how response inhibition contributes to
89 postural equilibrium (Cohen et al., 2011; England et al., 2021; Potocanac et al., 2014; Rydalch
90 et al., 2019; Sparto et al., 2012). The aforementioned studies focused on the execution of rapid
91 stepping, since change-of-support reactions are often needed to regain balance (Maki &
92 McIlroy, 1997). Older adults make more anticipatory postural adjustment errors during a
93 choice reaction voluntary step task compared with younger adults (Cohen et al., 2011). In this
94 case, initial acceptance of body load onto the wrong stance leg needed to first be corrected
95 before shifting weight onto the other leg to allow the step to proceed. This led to increased
96 choice-reaction times. Interestingly, the same study also revealed that Stroop task performance
97 correlated with anticipatory postural adjustment errors preceding the step. The authors
98 surmised that what may underlie an increased choice reaction time for older adults could in
99 fact be a deficit in response inhibition versus a generic drop in processing speed due to age.
100 Accordingly, Schoene et al. (2017) revealed that inhibitory choice reactive stepping time was
101 associated with falls independently of reduced processing speed, lack of attention, or balance
102 impairment. See Rey-Mermet et al. (2018), Rey-Mermet & Gade (2018), and Verhaeghen
103 (2011) for a more nuanced discussion on the topic of inhibitory deficits and ageing.

104 We have recently demonstrated that performance on a balance recovery step task was
105 correlated with speed of response inhibition in a computerised test of inhibitory control
106 (England et al., 2021; Rydalch et al., 2019). These results, holding true for both young and
107 older adults, suggest a common neural mechanism underlying inhibitory performance on a
108 seated task with finger responses and a whole-body postural response to regain balance (Okubo
109 et al., 2022).

110 The underlying mechanisms of response inhibition (Enz et al., 2021; Jana et al., 2020) has
111 received much attention in the field of cognitive psychology in a wide range of disorders
112 (Penadés et al., 2007; Slaats-Willemse et al., 2003; Whelan et al., 2012). Using neuroimaging

113 three underlying neural networks of response inhibition have been identified: the right inferior
114 frontal cortex (rIFC), the presupplementary motor area (preSMA), and the subthalamic nucleus
115 (STN) (Aron et al., 2007; Aron & Poldrack, 2006; Swann et al., 2012). Coxon et al. (2012)
116 demonstrated that these nodes, and the strength of connectivity between them, are related to
117 performance on response inhibition tasks. They showed that the integrity of white matter
118 connections between the rIFC and the STN predicted response inhibition task performance and
119 so did tract strength between preSMA and STN, but only in older adults.

120

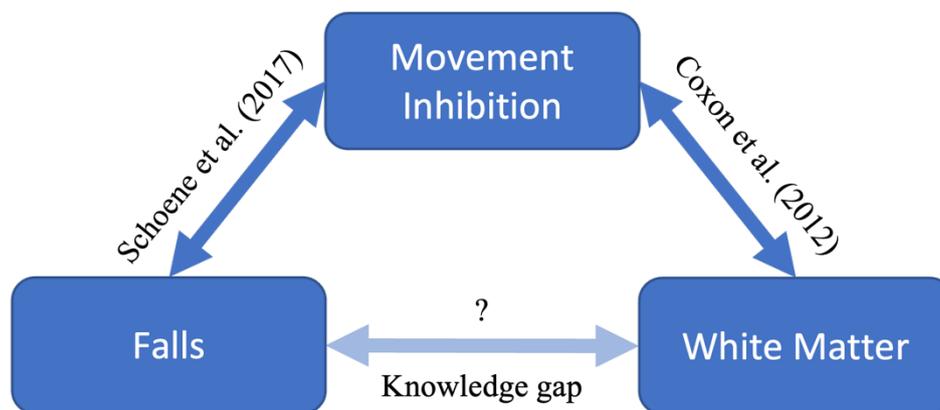


Figure 1. Theoretical framework. Schoene et al. (2017) have shown that improved performance on movement inhibition tasks are associated with a reduced number of falls in the real world. Coxon et al (2012) have shown that better performance on movement inhibition tasks is associated with higher fractional anisotropy (FA) in right IFC and stronger connectivity between left preSMA and left STN, only in older adults. We therefore tested whether individuals who fall less may show stronger white matter microstructure in the regions identified as key nodes for inhibitory control.

121 The theoretical framework has been outlined in Figure 1. We hypothesise that there will be an
122 association between white matter structures related to the motor inhibition network (STN,
123 preSMA, and right Inferior Frontal Gyrus - rIFG) and real world falls. The present study makes
124 use of an extensive data set from the Irish Longitudinal Study on Aging (TILDA), which is a
125 large-scale, longitudinal study with data on cognitive function, socioeconomic status,
126 education, health history and many other variables to provide insight into the aging process
127 from a broad perspective. Brain scans were collected from a subgroup (n=519) of TILDA
128 participants. These scans were used to analyse white matter microstructural integrity between
129 established nodes in the neural stopping network and determine if this was related to self-
130 reported falls. We predicted that individuals with diminished connectivity between these
131 specific networks would be more likely to experience falls. Overall, this study aims to provide

132 insight into the neural mechanism underlying a specific cognitive ability - inhibitory control -
133 and its relationship with fall prevalence in older adults.

134 2. Materials & methods

135 2.1 Participant recruitment

136 TILDA is a prospective, longitudinal cohort study that collects health, economic and social
137 data from a nationally representative sample of community-dwelling Irish residents aged 50
138 and over (Kearney et al., 2013). Ethical approval for the TILDA study was obtained from the
139 Faculty of Health Sciences Research Ethics Committee the Trinity College Dublin Research
140 Ethics Committee. Signed informed consent was obtained from all respondents prior to
141 participation. Additional ethics approval was received for the MRI sub-study from the St
142 James's Hospital/Adelaide and Meath Hospital, Inc. National Children's Hospital, Tallaght
143 (SJH/AMNCH) Research Ethic Committee, Dublin, Ireland. Those attending for MRI were
144 also required to complete an additional MRI-specific consent form.

145 We analysed participant data collected at waves 3, 4 and 5 of the study. The data collection
146 waves are approximately two years apart. Wave 1 was collected in 2009-2010, wave 2 was
147 collected in 2012, wave 3 was collected in 2014-2015, wave 4 was collected in 2016, and wave
148 5 was collected in 2018. A collection for wave 6 is currently ongoing.

149 Neuroimaging data was collected at wave 3 (Whelan & Savva, 2013). Of all participants
150 attending the wave 3 health assessment centre, a random subset were invited to return for multi-
151 parametric brain MRI at the National Centre for Advanced Medical Imaging (CAMI) at St
152 James's Hospital, Dublin. Participants with Mild Cognitive Impairment and stroke may exhibit
153 different fall profiles to those noted for typically ageing individuals and introduce additional
154 heterogeneity (Campbell & Matthews, 2010; Härlein et al., 2009; Lamb et al., 2003; Sheridan
155 & Hausdorff, 2007; Simpson et al., 2011). Therefore, we excluded participants with MOCA (<
156 20) or MMSE (< 24) scores at wave 3, and additionally individuals with history of stroke or
157 occurrence of stroke between data collection waves in the analysis.

158 Demographic variables applied as control variables in the models are presented in Table 1.
159 They include age, sex, medical history (Education levels, physical disability, Blood Pressure,
160 and polypharmacy), (Donoghue et al., 2018).

161

162 2.2 MRI protocol.

163 Participants were briefed on the MRI protocol ahead of acquisition, which comprised a variety
164 of scans including structural T1 weighted images and Diffusion Weighted Imaging (DWI)
165 sequences. Scans were acquired via 3T Philips Achieva system and 32-channel head coil.

166 For the T1 3D Magnetisation-prepared Rapid Gradient Echo (MP-RAGE) sequence the
167 acquisition parameters were: FOV (mm): 240 x 240 x 162; voxel size (mm): $0.8 \times 0.8 \times 0.9$;
168 SENSE factor: 2; TR: 6.7 ms; TE: 3.1 ms; flip angle: 8° ; acquisition time 5:24 minutes.
169 Diffusion Weighted Images (DWI) were acquired with 66 slices in transverse plane with field
170 of view 244 x 244 x 140mm; voxel size (mm): $1.9 \times 1.9 \times 2.0$; SENSE factor 2; TR: 12887
171 ms; TE: 55 ms; flip angle: 90° ; Diffusion was measured along 61 noncollinear directions ($b =$
172 1200 s/mm^2) preceded by a non-diffusion - weighted volume (reference volume, $b = 0 \text{ s/mm}^2$).
173 Total DWI acquisition time was 17:31 minutes.

174

175 2.3 DTI pre-processing

176 DWI data were processed using ExploreDTI (Leemans et al., 2009). Images were corrected for
177 subject motion and eddy currents using the procedure described in Leemans & Jones (2009).
178 Tensor estimation was performed using the iteratively reweighted linear least-squares approach
179 (Veraart et al., 2013). Fibre trajectories were computed with CSD based tractography (Tournier
180 et al., 2007) using recursive calibration of the response function to optimise the estimation of
181 the fibre orientation distribution (FOD) functions (Tax et al., 2014). A uniform grid of
182 tractography seed points at a resolution of $2 \times 2 \times 2 \text{ mm}^3$ was used with an angle threshold of
183 30 degrees, an FOD threshold of 0.1, and maximum harmonic order of eight. The median
184 number of streamlines computed for each participant was 55,221 (IQR 8665). A restricted
185 tractography analysis was performed subsequently to reconstruct streamlines passing through
186 pairs of ROIs that form part of the Shen 268 atlas (Shen et al., 2013). Reconstructed fibre
187 trajectories for each individual were quantified in terms of the (median) fractional anisotropy
188 (FA), Apparent Fibre Density (AFD), mean diffusivity (MD), and radial diffusivity (RD),
189 which are all measures that reflect the directional coherence of intracellular water diffusion.
190 Using Constrained Spherical Deconvolution for tractography rather than the traditional
191 diffusion tensor model allows calculation of the Apparent Fibre Density (AFD), a measure of
192 microstructural white matter integrity that performs better than standard Fractional Anisotropy
193 (FA) in regions with densely crossing fibres (Dell'Acqua & Tournier, 2019). As AFD provides

194 a superior measure, we focussed our inferential statistics on this metric, but have provided
195 comparable results with FA in the supplementary material for completeness and to allow
196 comparison with previous research studies.

197

198 2.4 Statistical Analysis Demographic Variables

199 Statistical analysis of the demographic variables at wave 3 were performed using independent
200 two-sample t-tests for age, sex, disability and number of medications, and chi-square tests for
201 the variables education, hypertension, and physical activity.

202

203 2.5 Logistic Regression

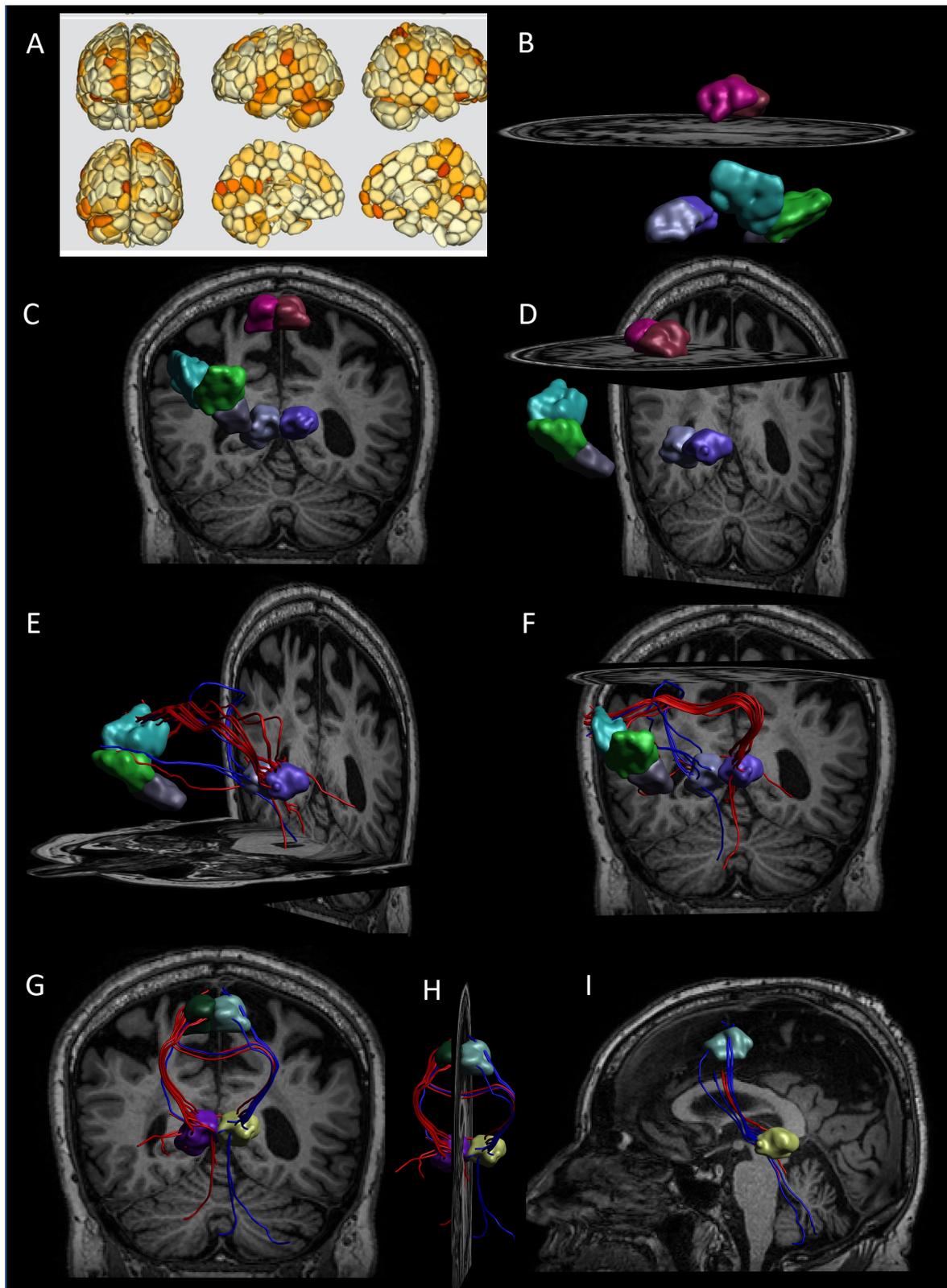
204 A logistic regression model was used to investigate the association between white matter
205 structures connecting selected regions of interest (ROI) and whether older individuals reported
206 falling. The model was created in RStudio (RStudio Team, 2022). For each ROI a logistic
207 model was generated. The binary dependent variable was whether participants had a fall (1) or
208 did not fall (0) between wave 3 (2014-2015) and wave 5 (2018). The independent variables of
209 interest were the respective measurements of reconstructed fibre trajectories for each ROI-ROI
210 pair. There were 6 independent control variables: Age, Sex, Education, Number of Medications
211 (Polypharmacy), Blood pressure, and a measure of physical disability. The following
212 paragraphs will describe elements of the model and add a rationale for including them.

213 2.5.1 Regions of Interest

214 The Shen 268 atlas was used (Figure 2A-D), which is a parcellation of the brain into 268 areas
215 based on resting functional state data (Shen et al., 2013). We selected 5 ROIs representing the
216 movement inhibition network: the right inferior frontal gyrus (rIFG), the left and right
217 subthalamic nuclei (r/l STN), and the left and right presupplementary motor area (r/l preSMA,
218 see Figure 2 E-I). All ROIs except the IFG consisted of individual shen atlas ROIs. However,
219 the IFG ROI consists of 3 individual shen atlas ROIs. Therefore, results involving the IFG will
220 be further analysed by looking at the individual ROIs.

221 The tractographies were conducted between the r/l STN and the other ROIs (rIFG, r/l preSMA),
222 or between the individual ROIs of the IFG and the r/l STN, resulting in 6 comparisons every
223 time. Therefore, the significance threshold was adapted using a Bonferroni correction for six
224 tests yielding a new critical alpha of 0.0083.

225 The tractography was conducted in a hypothesis driven manner between restricted pairs of
226 nodes based upon structural networks known to mediate inhibitory control (Table 2). To allow
227 for comparisons between ROIs, the AFD values were z-transformed.



228

229 *Figure 2. Regions of Interest and Reconstructed Streamlines.* Panel A shows the Shen atlas parcellation that was
 230 used, with ROIs shown in Panels B-D selected for analysis. Panels E-F show different viewpoints of the ROIs
 231 with reconstructed streamlines passing between right and left STN and right IFG for one representative participant.
 232 Panels G,H and I show different viewpoints of reconstructed streamlines passing between bilateral STN and
 233 preSMA.

234 *2.5.2 Control Analysis*

235 As an additional experimental control a separate tractography analysis between selected control
236 regions and the r/l STN was performed. As a control region for the rIFG, the left IFG was
237 chosen for topographical similarity but different functionality (Amunts & Zilles, 2012; Aron
238 et al., 2014; Deng et al., 2017; Du et al., 2020). For the r/l preSMA control region, we chose
239 the r/l FFA as a pair of symmetrical areas not related to movement inhibition (Burns et al.,
240 2019). Table 1 in the supplementary material describes the ROI characteristics.

241 *2.5.3 Control variables*

242 We included 6 control variables known to influence fall rates in our original logistic regression
243 model: Age, Sex, Education, Blood Pressure, Disability Score and Polypharmacy. An
244 additional variable of physical activity was added for the post-hoc analysis of the results. Age
245 is known to increase fall rate and was left untransformed as a numerical value (Chang et al.,
246 2015; Deandrea et al., 2010; Franse et al., 2017; Karlsson et al., 2013). Female sex increases
247 the severity of falls due to more prevalent osteoporosis and may increase fallrate, although the
248 findings on the latter are inconsistent (Deandrea et al., 2010; Franse et al., 2017; Karlsson et
249 al., 2013). Education is known to correlate with a wide array of neurologically relevant
250 characteristics. Education serves as an indirect measurement of socioeconomic status aside
251 from its protective effects against neurodegeneration. Both socioeconomic status and
252 neurodegenerative processes have been discussed in their relation to falls in the older
253 population (Khalatbari-Soltani et al., 2021; Then et al., 2016). In the linear models education
254 was coded as a numeric variable with numbers 1-3 for primary, secondary and tertiary
255 education.

256 Blood Pressure (BP) measurements were categorised after clinical criteria. For
257 Systolic BP the four thresholds were: Normal <120, Elevated < 130, Hypertension 1 < 140,
258 Hypertension 2 > 140 , and for Diastolic the four thresholds were: Normal <80, Elevated < 80,
259 Hypertension 1 < 89, Hypertension 2 > 90. If an individual presented two different
260 categorisation for systolic and diastolic blood pressure, the higher BP category was chosen.
261 High blood pressure may protect against falls caused by syncope due to low blood pressure
262 (Butt et al., 2012), however, contradictory results exist (Ha et al., 2021).

263 Physical disabilities are known to increase fall rates. Our disability score, recorded in
264 TILDA as a series of 11 self-reported yes or no questions asking if the respondent has difficulty
265 performing certain tasks (e.g. “Do you have difficulty walking 100m?”, or “Do you have

266 difficulty walking up 1 flight of stairs without resting”), was summed for each participant
267 resulting in a score of 1-12 (Deandrea et al., 2010; Ha et al., 2021). Different types of drugs,
268 such as antihypertensives, antiepileptics, sedatives and psychotropics are known to affect fall
269 rate. Therefore, the number of medicines used by a participant was included in the model as
270 measure of medicinal drug use (Bloch et al., 2011; Deandrea et al., 2010; Hartikainen et al.,
271 2007).

272 For an additional analysis the variable of physical activity was used. Physical activity
273 was coded per the IPAC standard (Craig et al., 2003). The IPAC asks participants to note the
274 amount of time they spent doing vigorous, moderate or walking activities and gives them
275 different weights to calculate a score and categorise participants into high, moderate and low
276 physical activity.

277 2.5.4 Predictive Model

278 For the logistic model aiming to predict future falling, fallers at wave 3 were removed, and
279 fallers at wave 4 and 5 were aggregated and labelled “fallers after wave 3”. Other parameters
280 were the same as for the cross-sectional model.

281 3. Result

282 3.1 Demographics

283 Fallers had a significantly higher number of disabilities $t(412) = 2.3738$, $p = 0.018$, and a
284 significant difference in the proportion of blood pressure categories between groups, $X^2(3) =$
285 17.0452 , $p = 0.00069$. The significant result for blood pressure is driven by hypertension 1.
286 Without Hypertension 1 the result loses significance $X^2(2) = 0.25$, $p = 0.88$.

288 For the cross-sectional analysis our criteria resulted in the inclusion of 414 participants that
 289 underwent MRI acquisition at wave 3. Ninety seven of the 414 participants at wave 3 reported

Table 1

Demographic variables of selected participants at wave 3

			Fallers W3 (n = 97)	Nonfallers W3 (n = 317)	p-Value
Age		Mean (sd)	69.21 (8.23)	68.2 (7.39)	0.2524 ^b
Sex	Male	n (%) ^a	42 (43.3)	158 (49.8)	0.31 ^c
	Female	n (%) ^a	55 (56.7)	159 (50.2)	
Education					0.29 ^c
	Level 1	n (%) ^a	22 (22.7)	51 (16.1)	
	Level 2	n (%) ^a	36 (37.1)	119 (37.5)	
	Level 3	n (%) ^a	39 (40.2)	147 (46.4)	
Disability		Mean (sd)	2.05 (1.88)	1.58 (1.65)	0.018 ^b
Blood Pressure					0.00069 ^c
	Normal	n (%) ^a	25 (25.8)	69 (21.8)	
	Elevated	n (%) ^a	16 (16.5)	39 (12.3)	
	Hypertension 1	n (%) ^a	10 (10.3)	99 (31.2)	
	Hypertension 2	n (%) ^a	46 (47.4)	110 (34.7)	
Number of Meds		Mean (sd)	2.94 (2.34)	2.5 (2.52)	0.13 ^b
Physical Activity		n	92	302	0.21 ^c
	Low	n (%) ^a	35 (38.0)	106 (35.1)	
	Moderate	n (%) ^a	40 (43.5)	113 (37.4)	
	High	n (%) ^a	17 (18.5)	83 (27.5)	

Table 1. Table showing the basic demographic variables of participants at wave 3 selected for this study.

Participants were grouped into fallers and nonfallers. ^a Valid percent ^b Independent two-sample t-test ^c Chi-square test over all levels and categories.

290 having fallen since the last interview. For the predictive analysis our criteria resulted in the
 291 inclusion of 317 participants of which 96 fell between waves 3 and 4, or between waves 4 and
 292 5.

293 3.3 Associative (cross-sectional) logistic regression results

294 The results of the cross-sectional logistic regression are depicted in Table 2. The model using
 295 the AFD values between the rIFG and rSTN achieved a p value of 0.005. This implies that an
 296 increase in AFD of 1 standard deviation in the tracts connecting rIFG and rSTN significantly
 297 increased the odds of falling by 1.49 (CI: 1.13, 1.98).

Table 2:

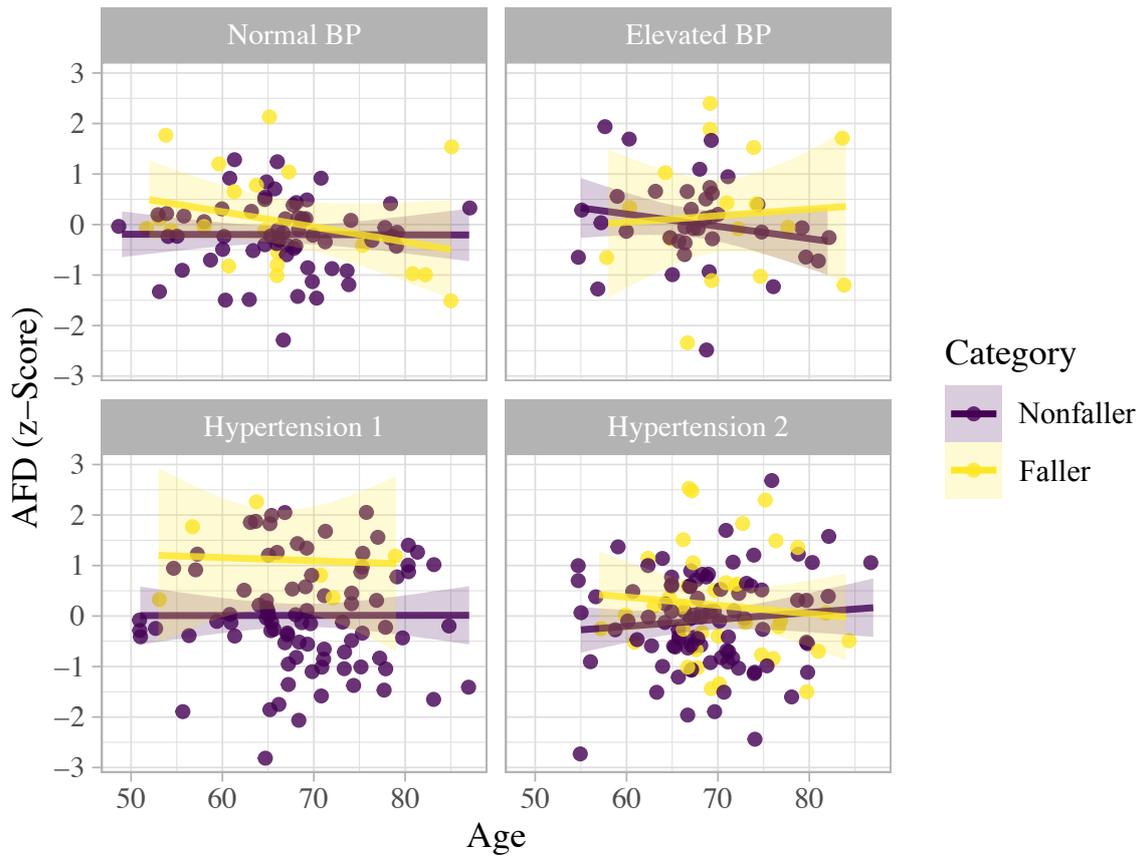
Association between microstructural integrity in inhibitory control networks and odds of falls in elderly.

Region	Odds	CI Low	CI High	P Value	Chi Square Fit	n
r IFG - r STN	1.49	1.13	1.98	0.005	0.00003	360
l preSMA - r STN	1.38	0.93	2.05	0.113	0.00046	200
r IFG - l STN	1.28	0.91	1.8	0.161	0.00172	237
r preSMA - r STN	0.84	0.61	1.16	0.288	0.02334	257
r preSMA - l STN	0.91	0.65	1.26	0.557	0.00976	228
l preSMA - l STN	0.97	0.73	1.29	0.855	0.00096	343

Table 2. Results of a logistic regression showing the association between the tractography of ROIs and the risk of falling in older people. A single result (r IFG to r STN) is significant after correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083), in bold. The Chi Square and number of observations in the model are included.

298 The model fulfilled all assumptions for a logistic regression (see supplementary material 5.2).
 299 A Chi square fit showed that the model was a good fit for the data ($\chi^2 = 0.00003$), and the
 300 McFadden R^2 Improved from 0.054 (model without AFD) to 0.094 by including the variable
 301 of interest. An additional observation is that the control variable blood pressure with category
 302 hypertension 1 significantly decreased the odds of falling by 0.18 (CI: 0.065, 0.48, p-value:
 303 0.00067) (Figure 3).

rIFG rSTN: AFD Value by Age

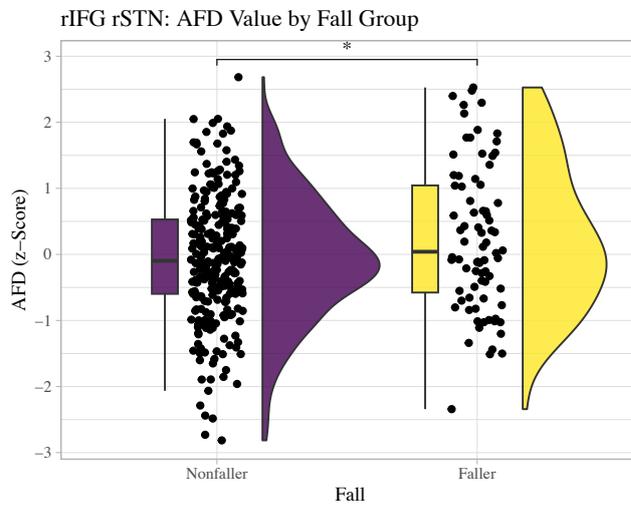


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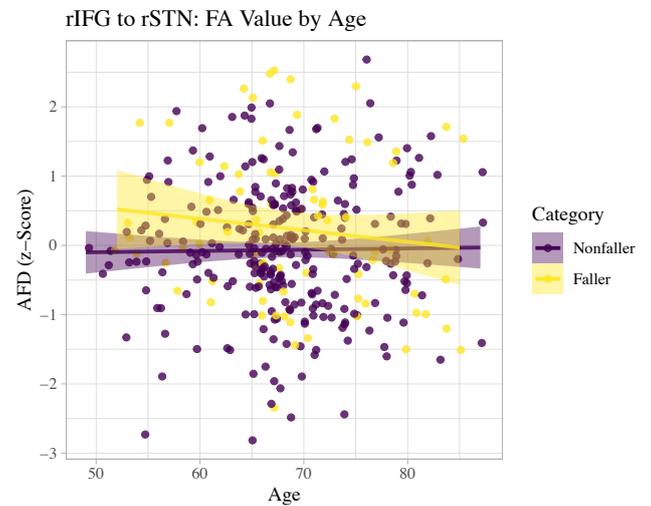
305 *Figure 3.* Figure 3 shows rIFG – rSTN fibre density (AFD) by Age, separated by Blood Pressure categories, with
 306 separate lines for fallers and nonfallers . There were significantly less fallers in the ‘Hypertension 1’ category. In
 307 the cohort with normal blood pressure, there are a total of 84 participants, 21 (25%) of which fell. For elevated
 308 blood pressure there are a total of 54 participants, 16 (29.63%) of which fell. For hypertension 1 there are a total
 309 of 93 participants, 6 (6.45%) of which fell. For hypertension 2 there are a total of 129 participants, 37 (28.68%)
 310 of which fell.

311 Figure 4A shows that older individuals who fell ($M = 0.23$, $SD = 1.1$) had higher AFD values
 312 in the white matter pathways connecting rIFG to rSTN (Nonfallers $M = -0.066$, $SD = 0.92$,
 313 directional Wilcoxon Rank Sum test, $W = 9716$, $p = 0.035$). This effect was most pronounced
 314 in the 50-65yr old fallers, as AFD values appeared to be lower in the older 65+ fallers.
 315 Nonfallers show no such trend in AFD values cross sectionally over the age range. We
 316 investigated this post hoc by adding an age-AFD interaction term to the rIFG-rSTN model. The
 317 age-AFD interaction term did not reach significance, reducing odds of a fall by 0.038 (CI:
 318 0.072, 1.28, $p = 0.058$) while the AFD term was still significant, increasing the odds of a fall
 319 by 21.87 (CI: 16.47, 29.04, $p = 0.03$). The increase in odds for the rIFG to rSTN AFD value is
 320 mathematically inflated in the model with the interaction term, as the value features twice in
 321 the model as part of the interaction and main effect. It is also further inflated due to the
 322 comparatively high numeric range of age.

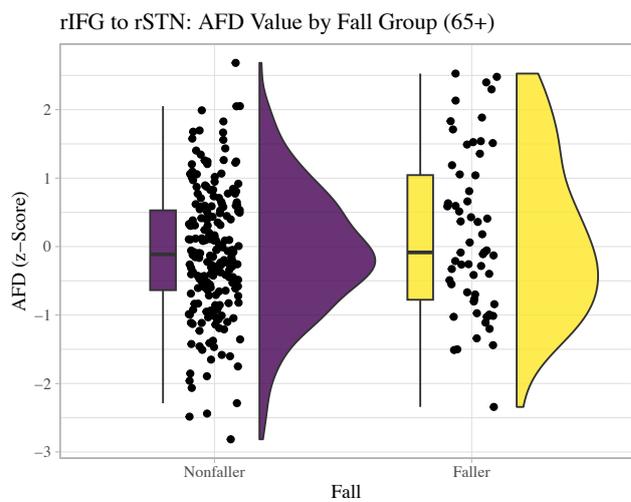
A



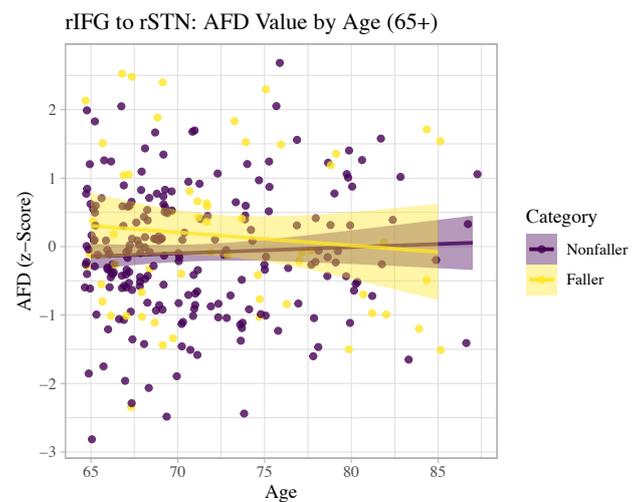
B



C



D



324 *Figure 4.* Figure A shows differences in the distribution of fallers vs nonfallers. Fallers seem to have overall higher
 325 AFD values. Figure B shows the difference in distribution according to age. Fallers also have a higher average
 326 AFD value, although this relationship is dependent on age. Figure C and D show the difference in distribution of
 327 fallers, but only including fallers of age 65 or more.

328

329 Constraining the analysis to individuals aged 65 + has no effect on the overall distribution
 330 (Figure 4 C & D). However, no significant results were found using a sample of people aged
 331 65 or more – likely due to the reduced sample size.

Table 3:

Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
rIFG - r STN	2.31	1.42	3.78	0.00082	0.000061	360
l preSMA - r STN	1.31	0.74	2.3	0.35	0.0098	200
l preSMA - l STN	1.23	0.76	2	0.41	0.0037	343
r preSMA - l STN	0.8	0.43	1.49	0.48	0.041	228
r preSMA - r STN	0.83	0.47	1.47	0.53	0.1	257
rIFG - l STN	1.06	0.61	1.86	0.83	0.0083	237

Table 3. Results of a logistic regression showing the association between the tractography of ROIs and the risk of falling in older people when accounting for physical activity. A result (r IFG to r STN) is significant after correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083), the pis bold. The Chi Square and number of observation of the model are included.

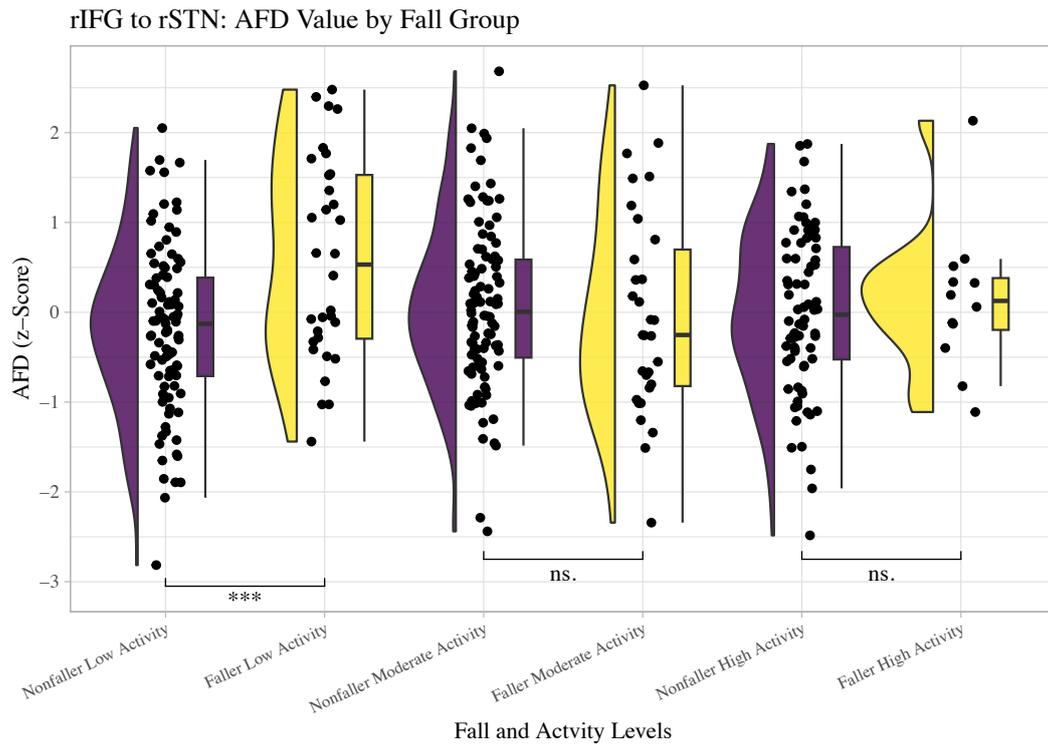
333 We hypothesized that higher AFD values indicative of dense white matter connectivity in older
 334 people would be associated with lower risk of falling. However, this relationship was not found
 335 in our data – instead, we found that higher AFD led to increased fall risk. We investigated this
 336 relationship deeper, hypothesizing that more active older people may be generally healthier
 337 and have higher AFD values, and be more likely to fall due to greater physical activity than
 338 their sedentary counterparts.

339 Adding an interaction between physical activity level and AFD values to the model required
 340 the inclusion of a main effect term. Therefore, the updated logistic regression model contained
 341 two new elements; a term for physical activity and the term for the interaction between physical
 342 activity and AFD values.

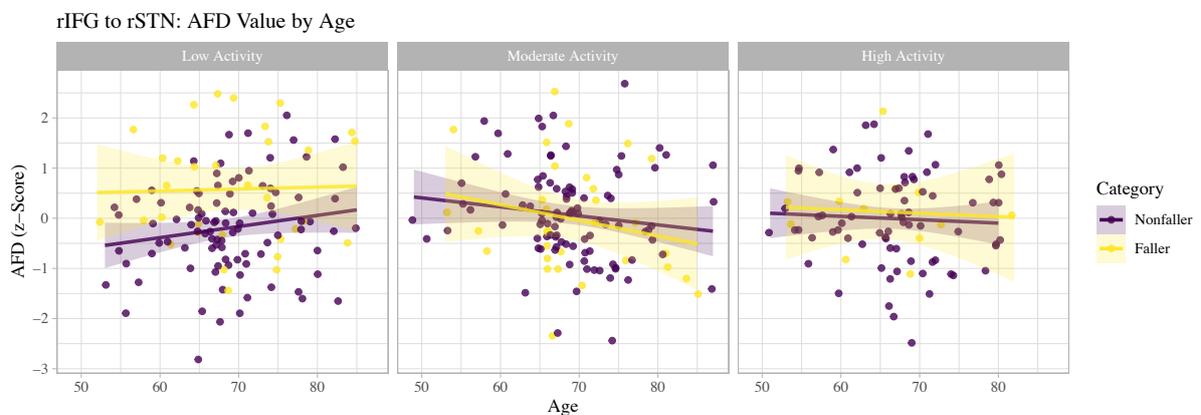
343 The results of the cross-sectional logistic regression are depicted in Table 3. The model using
 344 the AFD values between the rIFG and rSTN achieved a p value of 0.00082. This means that an
 345 increase in rIFG - rSTN AFD by 1 standard deviation significantly increased the odds of falling
 346 by 2.31 (CI: 1.42, 3.78). The McFadden Pseudo R squared of this model improves to 0.12
 347 compared to a model with no AFD and no AFD * physical activity interaction.

348 Moderate physical activity increased the odds of falling by 1.44 (CI: 0.75, 2.75),
 349 although not significantly (p= 0.28). However, the interaction term of moderate physical
 350 activity and AFD value significantly (p= 0.014) decreased the odds of falling by 0.44 (CI: 0.22,
 351 0.84). High physical activity does not significantly affect outcomes, neither as a main or
 352 interaction effect.

A



B



353 *Figure 5.* Panel A shows differences in the distribution of fallers vs nonfallers. Fallers have overall higher AFD
 354 values in the low activity condition, but not in high or moderate physical activity. Figure B shows the difference
 355 in distribution according to age. Fallers also have a higher average AFD value, and this relationship is less
 356 dependent on age when accounting for physical activity.

357

358 In Figure 5 it is visible that AFD is significantly ($t(125) = -3.87, p = 0.00018$) higher
 359 for fallers ($m = 0.58, sd = 1.12$; nonfallers = $m = -0.19, sd = 0.92$) that are not physically active,
 360 however, the same is not true for moderately active (Fallers: $m = -0.023, sd = 1.13$; nonfallers:
 361 $m = 0.066, sd = 0.92$; $t(127) = 0.44, p = 0.66$), or highly active older people (Fallers: $m = 0.13,$

362 sd = 0.82; nonfallers: m = -0.007, sd = 0.9; t(86) = -0.5, p= 0.62). The data presented in Figure
 363 5B further suggests that much of the interaction between falling and age is cleared up when the
 364 model accounts for physical activity.

365 *3.3.1.1 ROI Subregion Analysis*

Table 4:

Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

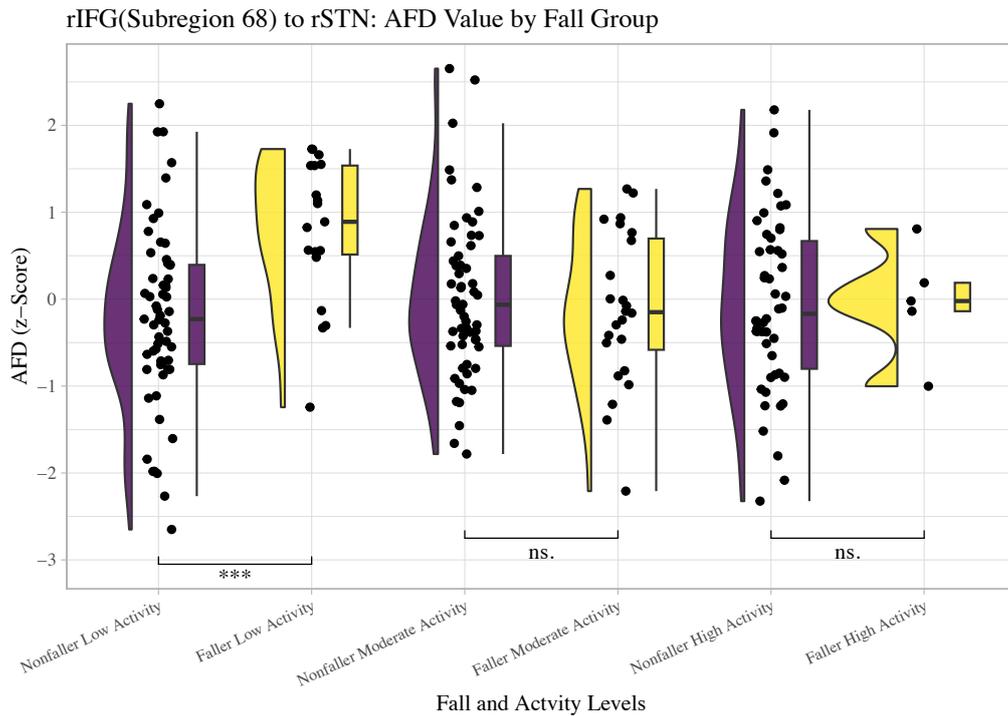
Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
rIFG (subregion 68) - r STN	3.59	1.7	7.56	0.00079	0.000027	221
rIFG (subregion 79) - r STN	2.08	1.06	4.05	0.032	0.007	249
rIFG (subregion 79) - l STN	1.79	0.84	3.8	0.13	0.16	130
rIFG (subregion 90) - r STN	0.58	0.28	1.19	0.14	0.21	186
rIFG (subregion 68) - l STN	1.22	0.45	3.31	0.7	0.0016	139
rIFG (subregion 90) - l STN	8.93E+21	0	-	1	0.0014	35

Table 4. Results of a logistic regression showing the association between the tractography of ROIs and the risk of falling in older people when accounting for physical activity. A result (r IFG to r STN) is significant after correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083), the pis bold. The Chi Square and number of observation of the model are included.

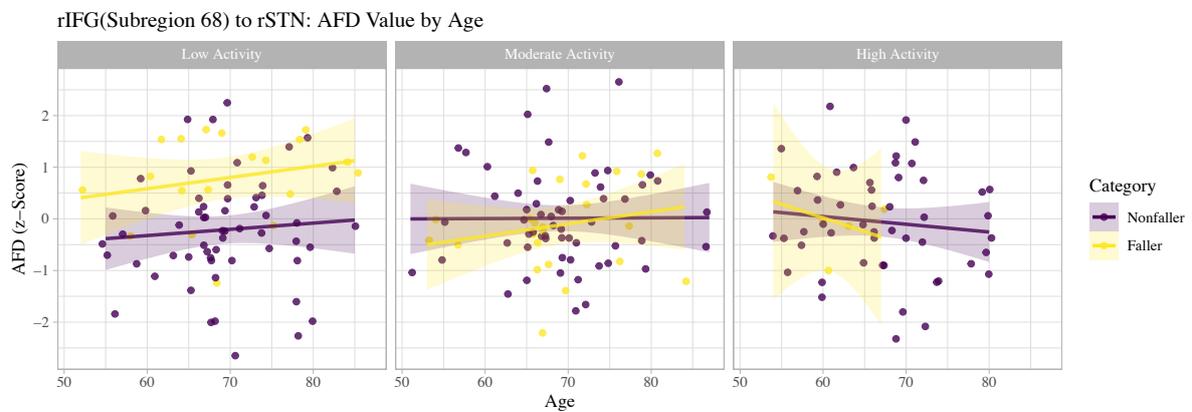
366
 367 The results of the cross-sectional logistic regression testing three further sub-divisions of rIFG
 368 are depicted in Table 4. When analysing subregions of the rIFG, one region is significant. Area
 369 68 - R.BA.37.10 in the Shen atlas – near to the parahippocampal gyrus is significant (p=
 370 0.00079). Increases of 1 SD of AFD in this region increases the odds of falling by 3.59 (CI:
 371 1.7, 7.56).

372

A



B



373 *Figure 6.* Figure A shows differences in the distribution of fallers vs non fallers. Fallers seem to have overall
374 higher AFD values in the low activity condition, but not in high or moderate physical activity. Figure B shows the
375 difference in distribution according to age. Fallers also have a higher average AFD value.

376

377 Compared to the model using the whole rIFG structure, the McFadden pseudo R squared
378 improves from 0.054 in a model with no AFD or AFD and physical activity interaction term to
379 0.2.

380 In this model, moderate physical activity significantly increased the odds of falling by 2.6 (CI:
381 1.05, 6.4, $p=0.038$). Similarly, the interaction term of moderate physical activity and AFD

382 value significantly ($p= 0.006$) decreased the odds of falling by 0.27 (CI: 0.1, 0.68). High
 383 physical activity did not significantly affect outcomes, neither as a main or interaction effect.

384 Looking at Figure 6 we can see that AFD is significantly ($t(76) = -3.85, p= 0.00025$) higher for
 385 fallers ($m = 0.79, sd = 0.83$; nonfallers: $m = -0.21, sd = 1.03$) that are not physically active,
 386 however, the same is not true for moderately active (Fallers: $m = -0.12, sd = 0.88$; nonfallers:
 387 $m = 0.012, sd = 0.94$; $t(79) = 0.59, p= 0.56$), or highly active older people (Fallers: $m = -0.033,$
 388 $sd = 0.65$; nonfallers: $m = 0.06, sd = 1$; $t(53) = -0.058, p= 0.95$).

389

390 3.4 Predicting future falling from structural brain data

391 We combined data on falling that occurred at any point following the MRI scan at wave 3 until
 392 wave 5. The results of the predictive logistic regression are depicted in table 5. AFD of white
 393 matter pathways connecting any of the aforementioned ROIs did not predict future falling at
 394 waves 4 or 5. (Table 5).

395 The results of the predictive logistic regression accounting for physical activity are depicted in
 396 table 6. No significant association between the independent and dependent variables were
 397 observed (Table 5).

Table 5:

Prediction of fall risk in older adults by white matter microstructure.

Region	Odds	CI Low	CI High	P Value	Chi Square Fit	n
l preSMA - l STN	1.42	1.05	1.92	0.023	0.023	265
r preSMA - r STN	0.74	0.52	1.06	0.097	0.017	200
r preSMA - l STN	0.81	0.54	1.2	0.29	0.026	171
r IFG - r STN	1.04	0.78	1.39	0.776	0.125	276
r IFG - l STN	0.97	0.66	1.42	0.861	0.330	180
l preSMA - r STN	0.98	0.69	1.4	0.926	0.387	156

Table 5. Results of a logistic regression showing the prediction of the risk of falling in older adults using Apparent Fibre Density in pathways connecting targeted ROIs. No result is significant after correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083). The Chi Square and number of observation of the model are included.

398

399

400

Table 6:

Association between microstructural integrity in inhibitory control networks and odds of falls in older adults

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
r preSMA - r STN	0.43	0.22	0.84	0.014	0.039	201
l preSMA - l STN	1.55	0.93	2.58	0.09	0.14	268
rIFG - r STN	1.16	0.74	1.84	0.52	0.28	282
rIFG - l STN	0.92	0.5	1.7	0.79	0.34	186
l preSMA - r STN	1.04	0.64	1.69	0.88	0.24	158
r preSMA - l STN	1.03	0.5	2.12	0.94	0.12	173

Table 6. Results of a logistic regression showing the prediction of the risk of falling in older adults using the Apparent Fibre Density. No result is significant after correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083). The Chi Square and number of observation of the model are included.

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3.5 Control ROI analysis

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To further guard against false positives, we also performed a control analysis using areas not directly implicated in inhibitory control. To maintain similarity with the experimental analyses, we still targeted bilateral STN, but instead of analysing the rIFG and preSMA connections to STN, we chose the FFA (Fusiform Face Area), an area generally not considered to be substantial components of the inhibitory control network. We also added the lIFG area (consisting of 3 shen ROIs). The lIFG was included to increase the validity of the control ROIs. However, as task challenge, age or impairment increase, lIFG may influence inhibitory performance (Heilbronner & Münte, 2013; Swick et al., 2008). This yielded no significant results when any of the aforementioned models were conducted with the control regions.

412

413

414

Voxel count (with rIFG and lIFG split up into their individual ROIs) between control ROIs (Mean = 3391, SD = 738.99) and experimental ROIs (Mean = 3919.86, SD = 899.14) did not differ significantly ($t(11.567) = 1.20, p = .25$).

415

3.5.1 Cross-Sectional Models for Control ROIs

416

417

The results of the cross-sectional logistic regression are depicted in table 3. No significant association between the independent and dependent variables were observed (Table 7).

Table 7

Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
r FFA - r STN	1.56	1.04	2.33	0.03	0.0227	178
lIFG - l STN	0.73	0.53	1	0.05	0.0001	282
lIFG - r STN	0.84	0.59	1.21	0.36	0.0042	197
l FFA - l STN	0.85	0.54	1.35	0.5	0.0050	124
r FFA - l STN	1.34	0.44	4.08	0.61	0.2286	39
l FFA - r STN	0.92	0.42	2	0.83	0.0192	70

Table 7. Results of a logistic regression showing the prediction of the risk of falling in older adults using the Apparent Fibre Density. No result is significant after correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083). The Chi Square and number of observation of the model are included.

418 *3.5.1 Predictive Models for Control ROIs*

419 The results of the predictive logistic regression are depicted in table 8. No significant
 420 association between the independent and dependent variables were observed (Table 8).

Table 8

Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
l IFG - l STN	1.38	1	1.91	0.05	0.0015	223
r FFA - l STN	0.34	0.09	1.3	0.12	0.1150	29
r FFA - r STN	1.37	0.89	2.09	0.15	0.0081	138
l FFA - r STN	1.42	0.73	2.78	0.3	0.2500	55
l FFA - l STN	0.99	0.54	1.84	0.98	0.1232	89
l IFG - r STN	1	0.65	1.53	1	0.1557	147

Table 8. Results of a logistic regression showing the prediction of the risk of falling in older adults using Apparent Fibre Density. No result is significant after correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083). The Chi Square and number of observation of the model are included.

421

4. Discussion

422 In the current longitudinal investigation we demonstrated a significant association between
423 white matter fibre density in pathways connecting two key regions in the brain's inhibitory
424 control network, and falling in a large sample (n=414) of older participants. We tested the
425 microstructural integrity of white matter pathways corresponding to the direct and hyperdirect
426 cortical-subcortical loops implicated in inhibitory control, and found that only connectivity
427 between right Inferior Frontal Gyrus (rIFG) and right Subthalamic Nucleus (rSTN) was
428 implicated in falling. This was observed cross-sectionally by modelling self-reported falling
429 that had already occurred in the time period preceding structural brain measurements. The
430 rIFG-rSTN connectivity was not, however, predictive of future falling when measured two and
431 four years later. Further, no such relationships existed for selected control brain regions that
432 are not implicated in inhibitory control. While statistically robust and surviving strict multiple
433 comparison corrections, our key finding was counterintuitive as the direction of the effect was
434 opposite to that which we hypothesised. Higher Apparent Fibre Density (AFD) values in the
435 rIFG-rSTN pathways were associated with greater likelihood of falling. We performed post-
436 hoc analyses to unpick the effect further, revealing that this finding was significantly influenced
437 by physical activity levels in the older individuals. Higher AFD values only yielded higher
438 odds of falling in combination with low levels of physical activity. In individuals with moderate
439 or high physical activity levels, AFD had no bearing on falling.

440 Having a large sample size allowed us to construct a complex logistical model with falling as
441 the dependant variable, using a set of known influences as control variables (Age, sex,
442 education, blood pressure, polypharmacy, disabilities of daily living) and the AFD values
443 between ROIs as independent variables. We focussed our analysis on apparent fibre density
444 (AFD) instead of the traditionally reported FA values to measure white matter structures within
445 the brain. AFD offers several advantages over FA, the most pertinent being increased accuracy
446 for measuring crossing fibres tracts within voxels (Dell'Acqua & Tournier, 2019). The model
447 reaffirmed the previous finding that high blood pressure may act as a protective factor against
448 falls – likely by preventing falls due to syncope from blood pressure drops (Butt et al., 2012).
449 A further strength of the study was that an investigation into control areas not related to
450 movement inhibition yielded no significant results.

451 Coxon et al. (2012) initially established a relationship between right Inferior Frontal Cortex
452 (rIFC) white matter structure and decreased response inhibition time in young and older adults.
453 They additionally reported higher FA in white matter projections bilaterally between the IFC

454 and STN in older (but not younger) adults with fastest response inhibition times. Schoene et al.
455 (2017) demonstrated an association between step response inhibition and real life falls and
456 consistent with this idea, Nagamatsu et al. (2013) found hypo-activation in prefrontal brain
457 regions during a test of inhibitory control in individuals who fell more often. Hence, we
458 hypothesised that greater microstructural integrity of white matter pathways in these networks
459 may predict current and future falling. While we did detect a significant relationship, our
460 finding that the individuals with most densely connected pathways fell more was surprising.
461 Our approach was to use AFD in a move towards more complex models that take into account
462 the complexity of fibre density and directionality such as AFD, and this is notably different
463 from the method employed by Coxon et al (2012) where FA was the main measure of white
464 matter microstructure. However, we did verify that the same pattern of results reported here
465 holds true with FA (see supplementary material for analyses). Furthermore, while FA values
466 generally decline with increasing age, this relationship does not apply to AFD values (Choy et
467 al., 2020). Therefore, a complex relationship between AFD in traditional stopping networks
468 and falling behaviour is likely. It is also possible that the higher density connectivity we
469 detected is a structural correlate of a less efficient, diffuse signal recruiting more neural units
470 as compensation for resources extended beyond their limits, but this is merely conjecture.
471 Considering how older adults show more widespread brain activity compared to younger adults
472 (Seidler et al., 2010), our results may be consistent with the theory that more effort and neural
473 resources are required in the older brain to achieve the same task that younger brains
474 accomplish more effortlessly.

475 As this was an observational study and the predictive models yielded no significant findings,
476 we cannot infer causality or directionality in the relationship between fibre density and falling.
477 The fact that individuals who fall tended to already have higher fibre density in inhibitory
478 control pathways may be a cause or consequence of the falling. For example, it is conceivable
479 that increased AFD values in fallers may be related to increased attention to balance and active
480 learning processes subsequent to a fall, rather than being pre-existing. Follow-up MRI scanning
481 with the same cohort of participants may unpick this relationship further to disentangle whether
482 changes in rIFG-rSTN microstructure drive changes in falling or vice versa.

483 To define this relationship further, we investigated the mediating effects of physical activity.
484 By definition physical activity implies that people are engaging in behaviours that make falls
485 more likely. It is therefore not surprising that physical activity itself leads to an increase in
486 falling behaviour in our models. Interestingly there was no correlation between falling and

487 AFD in those with higher physical activity levels. This warrants follow-up investigation with
488 more objective measurement methodologies as the activity levels reported in TILDA rely on
489 self-reported activity levels within the last 7 days of interviewing, which has been shown to be
490 subject to over- and underestimation (Lee et al., 2011; Prince et al., 2008).

491 5. Conclusion

492 Using MRI and self-reported data from 414 participants from the Irish longitudinal study on
493 ageing we showed that higher microstructural integrity in white matter pathways connecting
494 the right inferior frontal gyrus and right subthalamic nucleus was associated with falling in
495 older adults. This relationship was pre-existing at the time of structural MRI data acquisition,
496 and therefore precludes establishing causality or directionality of the effect. Fibre density at
497 the time of MRI data collection did not predict future falling two or four years later. Follow-
498 up MRI data will be required in order to determine whether densely connected regions in the
499 inhibitory control network change over time in a manner correlated with falling, or whether
500 this relationship is purely cross-sectional, and perhaps mediated by a third currently undefined
501 factor.

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Demographic variables of selected participants at wave 3

			Fallers W3 (n = 97)	Nonfallers W3 (n = 317)	p-Value
Age		Mean (sd)	69.21 (8.23)	68.2 (7.39)	0.2524 ^b
Sex	Male	n (%) ^a	42 (43.3)	158 (49.8)	0.31 ^c
	Female	n (%) ^a	55 (56.7)	159 (50.2)	
Education					0.29 ^c
	Level 1	n (%) ^a	22 (22.7)	51 (16.1)	
	Level 2	n (%) ^a	36 (37.1)	119 (37.5)	
	Level 3	n (%) ^a	39 (40.2)	147 (46.4)	
Disability		Mean (sd)	2.05 (1.88)	1.58 (1.65)	0.018 ^b
Blood Pressure					0.00069 ^c
	Normal	n (%) ^a	25 (25.8)	69 (21.8)	
	Elevated	n (%) ^a	16 (16.5)	39 (12.3)	
	Hypertension 1	n (%) ^a	10 (10.3)	99 (31.2)	
	Hypertension 2	n (%) ^a	46 (47.4)	110 (34.7)	
Number of Meds		Mean (sd)	2.94 (2.34)	2.5 (2.52)	0.13 ^b
Physical Activity		n	92	302	0.21 ^c
	Low	n (%) ^a	35 (38.0)	106 (35.1)	
	Moderate	n (%) ^a	40 (43.5)	113 (37.4)	
	High	n (%) ^a	17 (18.5)	83 (27.5)	

779 *Table 1.* Table showing the basic demographic variables of participants at wave 3 selected for this study.
 780 Participants were grouped into fallers and nonfallers. ^a Valid percent ^b Independent two-sample t-test ^c Chi-
 781 square test over all levels and categories.
 782

Region	Odds	CI Low	CI High	P Value	Chi Square Fit	n
r IFG - r STN	1.49	1.13	1.98	0.005	0.00003	360
l preSMA - r STN	1.38	0.93	2.05	0.113	0.00046	200
r IFG - l STN	1.28	0.91	1.8	0.161	0.00172	237
r preSMA - r STN	0.84	0.61	1.16	0.288	0.02334	257
r preSMA - l STN	0.91	0.65	1.26	0.557	0.00976	228
l preSMA - l STN	0.97	0.73	1.29	0.855	0.00096	343

785 *Table 2.* Results of a logistic regression showing the association between the tractography of ROIs and the risk of
 786 falling in older people. A single result (r IFG to r STN) is significant after correcting for multiple comparisons

787 (Bonferroni, new p threshold: 0.0083), in bold. The Chi Square and number of observations in the model are
 788 included.

789

790

791 Table 3

792 Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
rIFG - r STN	2.31	1.42	3.78	0.00082	0.000061	360
l preSMA - r STN	1.31	0.74	2.3	0.35	0.0098	200
l preSMA - l STN	1.23	0.76	2	0.41	0.0037	343
r preSMA - l STN	0.8	0.43	1.49	0.48	0.041	228
r preSMA - r STN	0.83	0.47	1.47	0.53	0.1	257
rIFG - l STN	1.06	0.61	1.86	0.83	0.0083	237

793 *Table 3.* Results of a logistic regression showing the association between the tractography of ROIs and the risk
 794 of falling in older people when accounting for physical activity. A result (r IFG to r STN) is significant after
 795 correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083), the pis bold. The Chi Square and
 796 number of observation of the model are included.

797

798 Table 4

799 Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
rIFG (subregion 68) - r STN	3.59	1.7	7.56	0.00079	0.000027	221
rIFG (subregion 79) - r STN	2.08	1.06	4.05	0.032	0.007	249
rIFG (subregion 79) - l STN	1.79	0.84	3.8	0.13	0.16	130
rIFG (subregion 90) - r STN	0.58	0.28	1.19	0.14	0.21	186
rIFG (subregion 68) - l STN	1.22	0.45	3.31	0.7	0.0016	139
rIFG (subregion 90) - l STN	8.93E+21	0	-	1	0.0014	35

800 *Table 4.* Results of a logistic regression showing the association between the tractography of ROIs and the risk of
 801 falling in older people when accounting for physical activity. A result (r IFG to r STN) is significant after
 802 correcting for multiple comparisons (Bonferroni, new p threshold: 0.0083), the pis bold. The Chi Square and
 803 number of observation of the model are included.

804

805 Table 5

806 Prediction of fall risk in older adults by white matter microstructure.

Region	Odds	CI Low	CI High	P Value	Chi Square Fit	n
l preSMA - l STN	1.42	1.05	1.92	0.023	0.023	265
r preSMA - r STN	0.74	0.52	1.06	0.097	0.017	200
r preSMA - l STN	0.81	0.54	1.2	0.29	0.026	171
r IFG - r STN	1.04	0.78	1.39	0.776	0.125	276
r IFG - l STN	0.97	0.66	1.42	0.861	0.330	180
l preSMA - r STN	0.98	0.69	1.4	0.926	0.387	156

807 *Table 5.* Results of a logistic regression showing the prediction of the risk of falling in older adults using
 808 Apparent Fibre Density in pathways connecting targeted ROIs. No result is significant after correcting for

809 multiple comparisons (Bonferroni, new p threshold: 0.0083). The Chi Square and number of observation of the
 810 model are included.

811
 812
 813

814 Table 6

815 Association between microstructural integrity in inhibitory control networks and odds of falls in older adults

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
r preSMA - r STN	0.43	0.22	0.84	0.014	0.039	201
l preSMA - l STN	1.55	0.93	2.58	0.09	0.14	268
rIFG - r STN	1.16	0.74	1.84	0.52	0.28	282
rIFG - l STN	0.92	0.5	1.7	0.79	0.34	186
l preSMA - r STN	1.04	0.64	1.69	0.88	0.24	158
r preSMA - l STN	1.03	0.5	2.12	0.94	0.12	173

816 *Table 6.* Results of a logistic regression showing the prediction of the risk of falling in older adults using the
 817 Apparent Fibre Density. No result is significant after correcting for multiple comparisons (Bonferroni, new p
 818 threshold: 0.0083). The Chi Square and number of observation of the model are included.

819

820 Table 7

821 Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
r FFA - r STN	1.56	1.04	2.33	0.03	0.0227	178
lIFG - l STN	0.73	0.53	1	0.05	0.0001	282
lIFG - r STN	0.84	0.59	1.21	0.36	0.0042	197
l FFA - l STN	0.85	0.54	1.35	0.5	0.0050	124
r FFA - l STN	1.34	0.44	4.08	0.61	0.2286	39
l FFA - r STN	0.92	0.42	2	0.83	0.0192	70

822 *Table 7.* Results of a logistic regression showing the prediction of the risk of falling in older adults using the
 823 Apparent Fibre Density. No result is significant after correcting for multiple comparisons (Bonferroni, new p
 824 threshold: 0.0083). The Chi Square and number of observation of the model are included.

825

826 Table 8

827 Association between microstructural integrity in inhibitory control networks and odds of falls in older adults.

Region	Odds	CI Low	CI High	p-Value	Chi Square Fit	n
l IFG - l STN	1.38	1	1.91	0.05	0.0015	223
r FFA - l STN	0.34	0.09	1.3	0.12	0.1150	29
r FFA - r STN	1.37	0.89	2.09	0.15	0.0081	138
l FFA - r STN	1.42	0.73	2.78	0.3	0.2500	55
l FFA - l STN	0.99	0.54	1.84	0.98	0.1232	89
l IFG - r STN	1	0.65	1.53	1	0.1557	147

828 *Table 8.* Results of a logistic regression showing the prediction of the risk of falling in older adults using Apparent
829 Fibre Density. No result is significant after correcting for multiple comparisons (Bonferroni, new p threshold:
830 0.0083). The Chi Square and number of observation of the model are included.
831

832 Figures

833 Figure 1

834

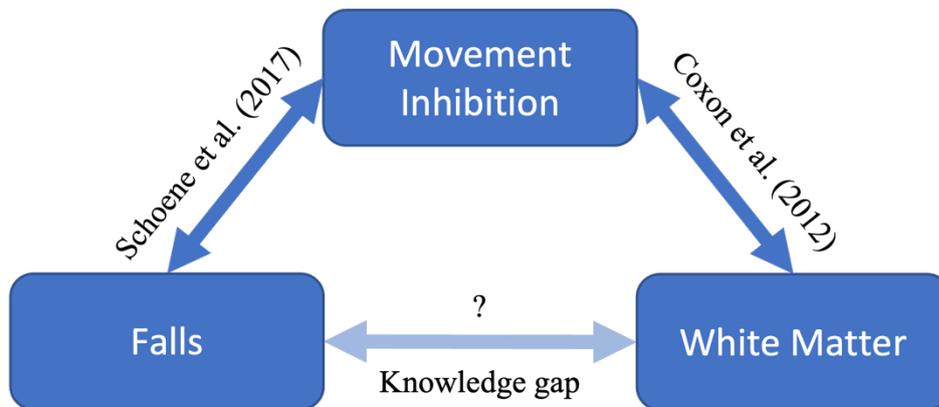
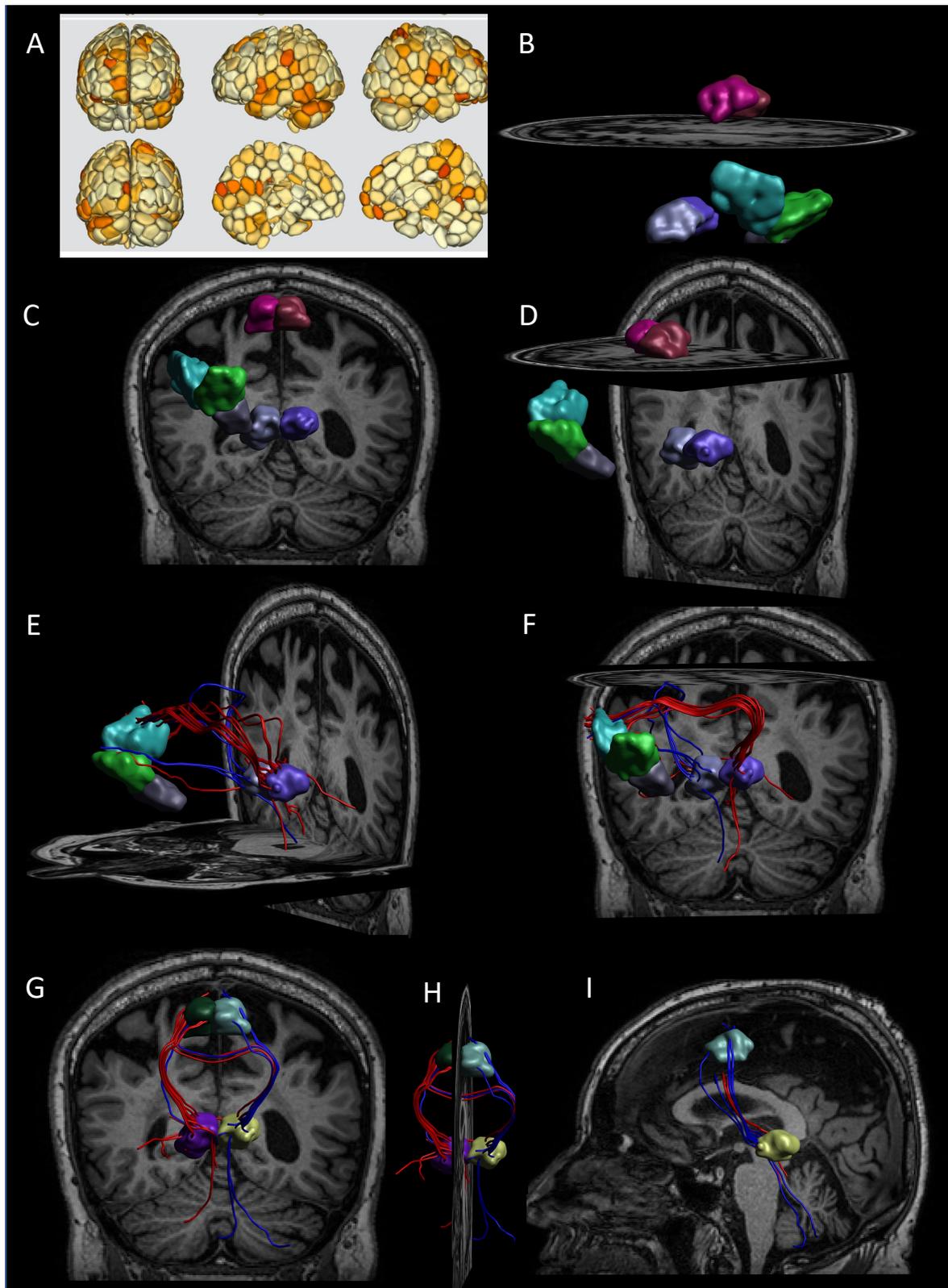


Figure 1. Theoretical framework. Schoene et al. (2017) have shown that improved performance on movement inhibition tasks are associated with a reduced number of falls in the real world. Coxon et al (2012) have shown that improved performance on movement inhibition tasks is associated with higher fractional anisotropy (FA) in right IFC and stronger connectivity between left preSMA and left STN, only in older adults. We therefore tested whether individuals who fall less may show stronger white matter microstructure in the regions identified as key nodes for inhibitory control.

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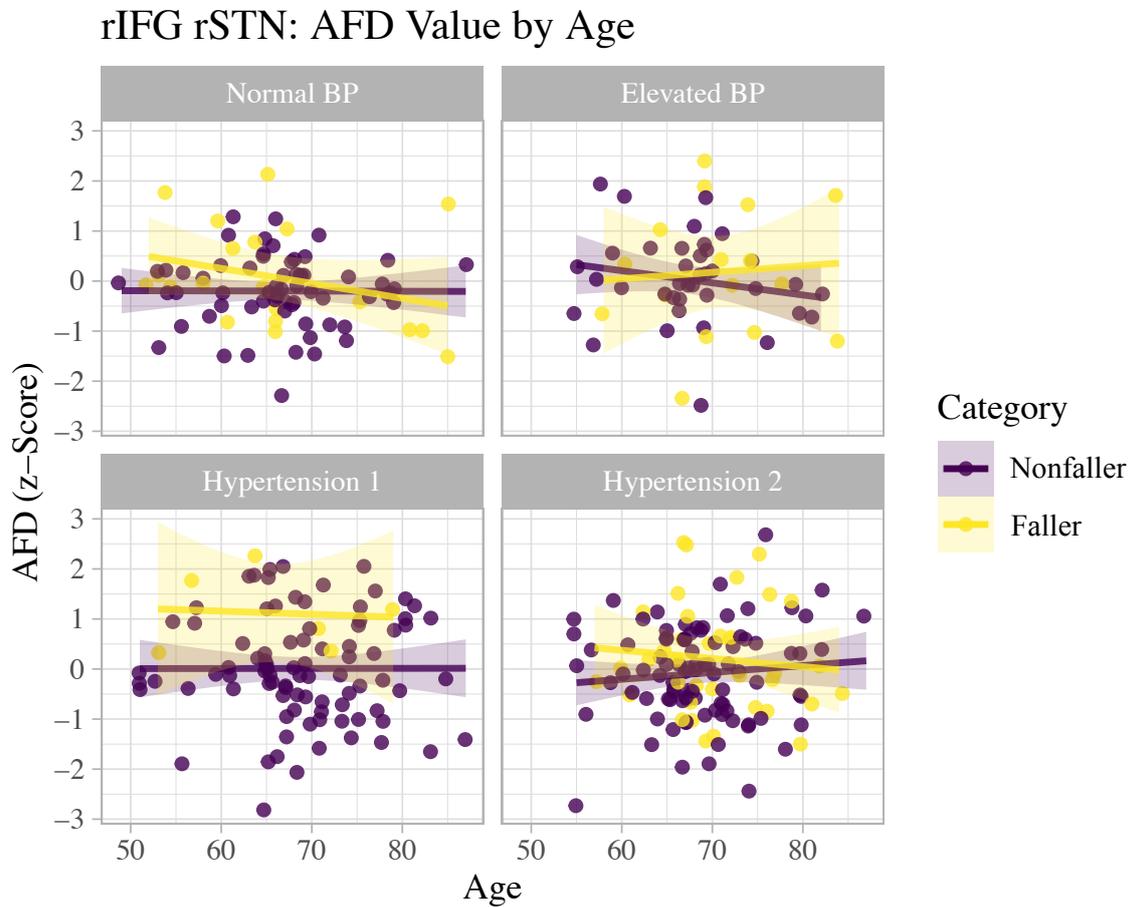


837

838 *Figure 2.* Regions of Interest and Reconstructed Streamlines. Panel A shows the Shen atlas parcellation that was
 839 used, with ROIs shown in Panels C-D selected for analysis. Panels E-F show different viewpoints of the ROIs
 840 with reconstructed streamlines passing between right and left STN and right IFG for one representative participant.

841 Panels G,H and I show different viewpoints of reconstructed streamlines passing between bilateral STN and
842 preSMA.

843 Figure 3

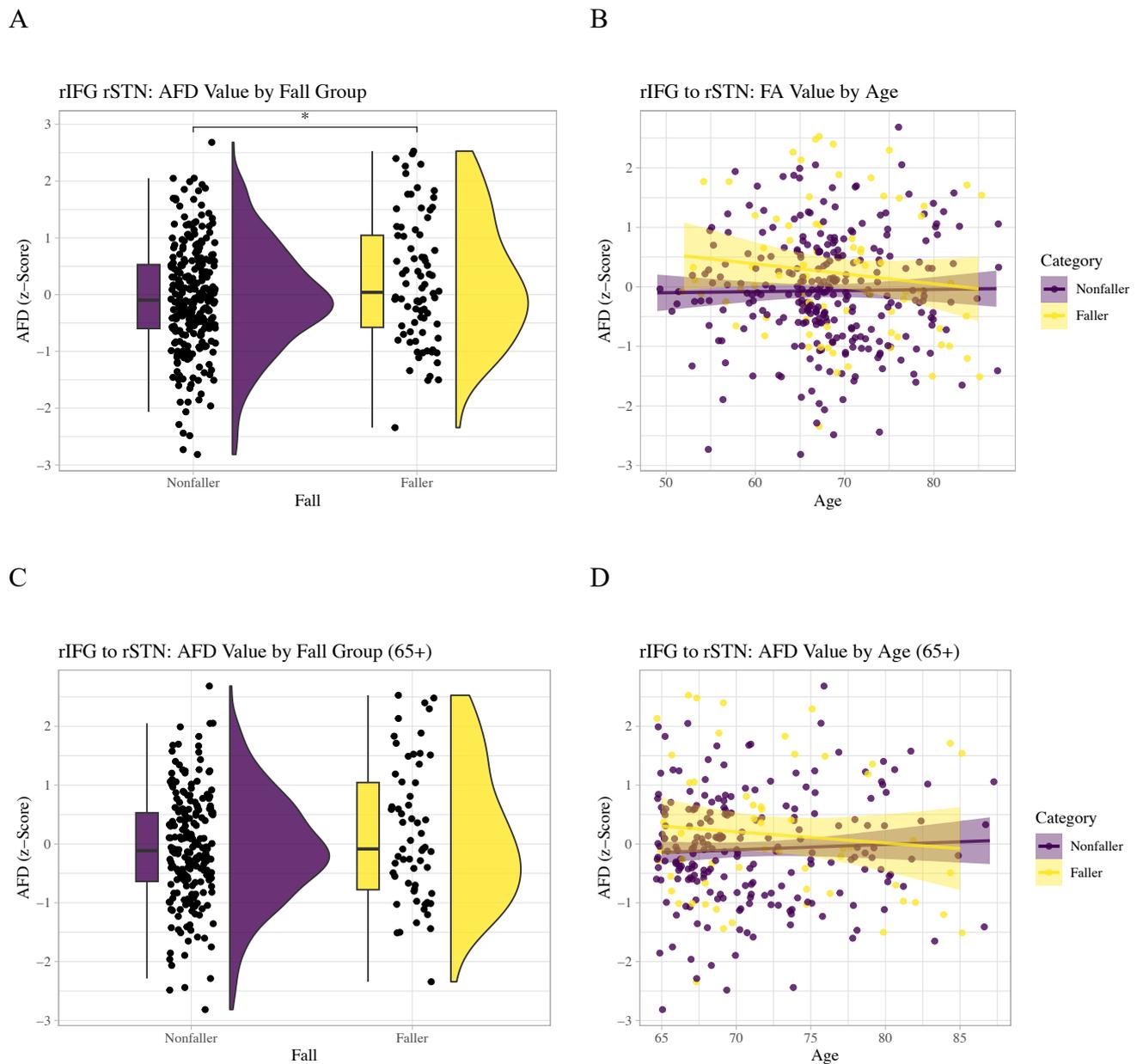


844

845 *Figure 3.* Figure 3 shows rIFG – rSTN fibre density (AFD) by Age, separated by Blood Pressure categories, with
846 separate lines for fallers and nonfallers . There were significantly less fallers in the ‘Hypertension 1’ category. In
847 the cohort with normal blood pressure, there are a total of 84 participants, 21 (25%) of which fell. For elevated
848 blood pressure there are a total of 54 participants, 16 (29.63%) of which fell. For hypertension 1 there are a total
849 of 93 participants, 6 (6.45%) of which fell. For hypertension 2 there are a total of 129 participants, 37 (28.68%)
850 of which fell.

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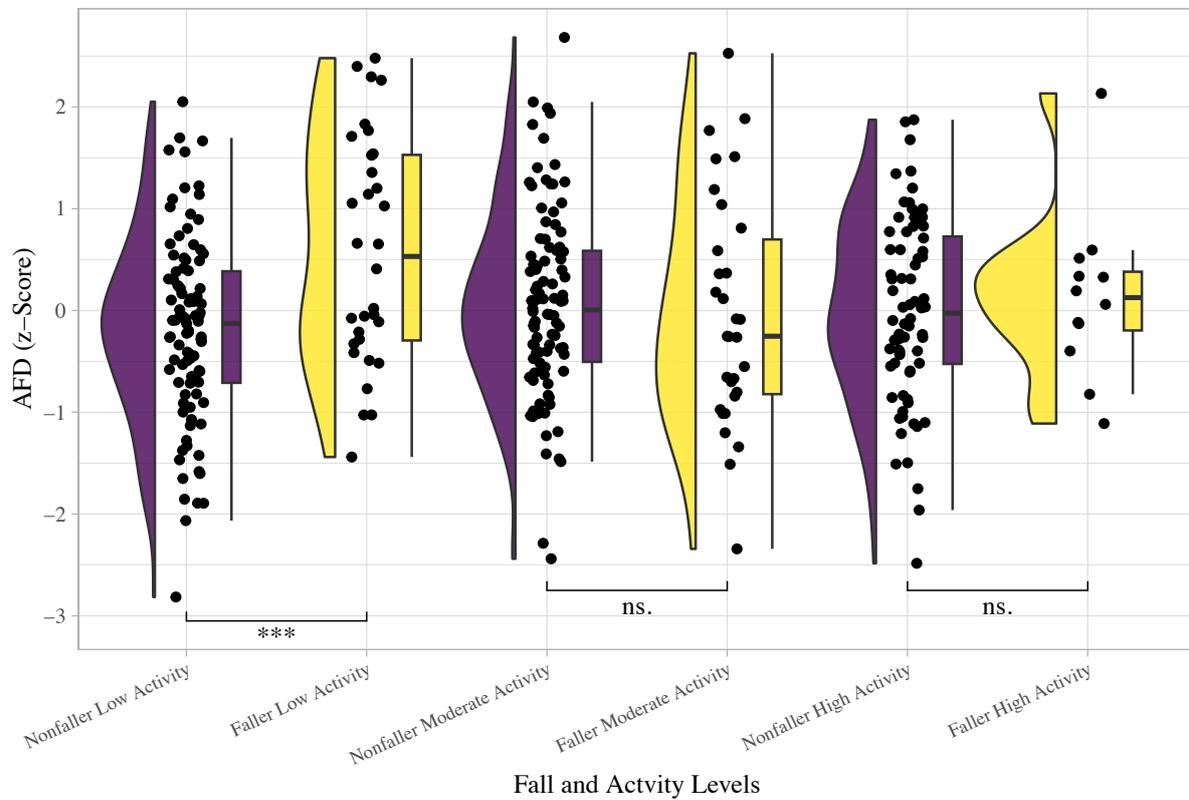
854 *Figure 4.* Figure A shows differences in the distribution of fallers vs nonfallers. Fallers seem to have overall higher
 855 AFD values. Figure B shows the difference in distribution according to age. Fallers also have a higher average
 856 AFD value, although this relationship is dependent on age. Figure C and D show the difference in distribution of
 857 fallers, but only including fallers of age 65 or more.

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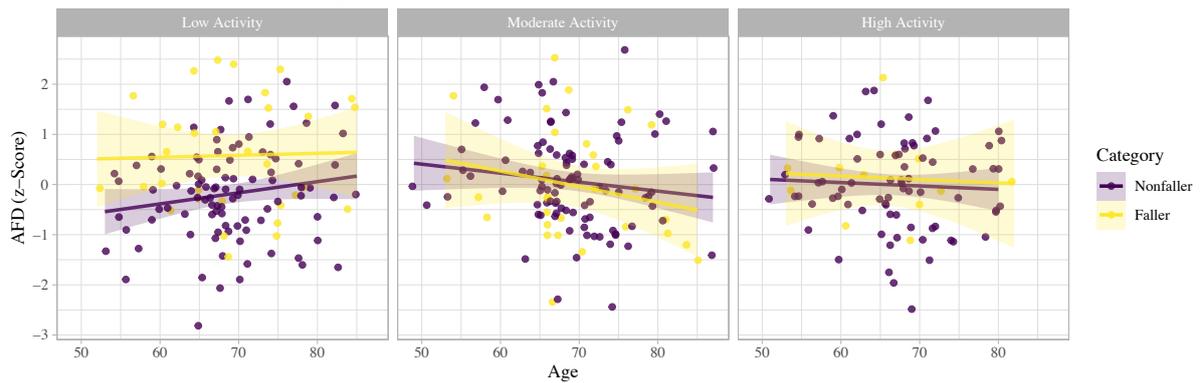
A

rIFG to rSTN: AFD Value by Fall Group



B

rIFG to rSTN: AFD Value by Age



861 *Figure 5. Panel A shows differences in the distribution of fallers vs nonfallers. Fallers have overall higher AFD*
862 *values in the low activity condition, but not in high or moderate physical activity. Figure B shows the difference*
863 *in distribution according to age. Fallers also have a higher average AFD value, and this relationship is less*
864 *dependent on age when accounting for physical activity.*

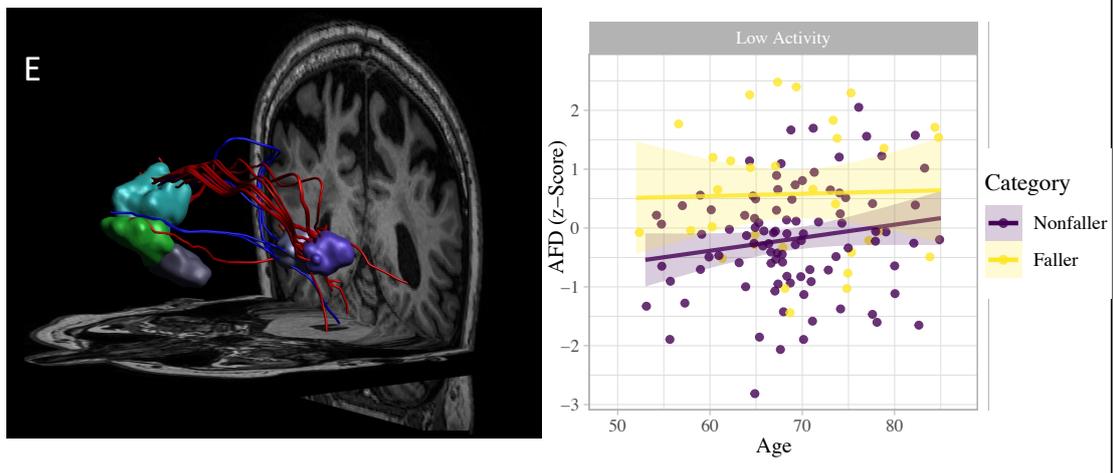
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866

White matter fibre density in the brain's inhibitory control network is associated with falling in older adults

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Recent research has indicated that the relationship between age-related cognitive decline and falling may be mediated by the individual's capacity to quickly cancel or inhibit a motor response. This longitudinal investigation demonstrates that higher white matter fibre density in the motor inhibition network paired with low physical activity was associated with falling in older adults.



871 Conflict of Interest Statement

872 The authors declare that the research was conducted in the absence of any commercial or
873 financial relationships that could be construed as a potential conflict of interest.

874 CRediT Contributions

875 Conceptualization: K.R. and D.B.; Data curation: S.K.; Formal analysis: C.S.; Funding
876 acquisition: K.R.; R.A.K, Methodology: C.S., K.R. and D.B.; Project administration: R.A.K,
877 C.S. and K.R.; Resources: S.K.; Software: C.S.; Supervision: K.R.; Visualization: C.S.;
878 Writing – original draft: C.S.; Writing - review & editing: C.S., K.R., D.B., J.M., R.A.K.,
879 V.A.S., C.D. and S.K.

880 Ethical Statement

881 Ethical approval for the TILDA study was obtained from the Faculty of Health Sciences
882 Research Ethics Committee the Trinity College Dublin Research Ethics Committee. Signed
883 informed consent was obtained from all respondents prior to participation. Additional ethics
884 approval was received for the MRI sub-study from the St James's Hospital/Adelaide and
885 Meath Hospital, Inc. National Children's Hospital, Tallaght (SJH/AMNCH) Research Ethic
886 Committee, Dublin, Ireland.

887

888 Data Availability Statement

889 The datasets generated during and/or analysed during the current study are not publicly available
890 due to data protection regulations but are accessible at TILDA on reasonable request. The
891 procedures to gain access to TILDA data are specified at <https://tilda.tcd.ie/data/accessing-data/>,
892 (accessed on 29th November 2023).

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