

Impacts of hydrodynamic conditions and surface roughness on the critical condition to develop and thickness of *Pseudomonas putida* biofilms

Guanju Wei¹ and Qingjun Judy Yang¹

¹University of Minnesota

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Abstract

The formation of biofilms can increase pathogenic contamination of drinking water, cause biofilm-related diseases, and alter the rate of sediment erosion in rivers and coasts. Meanwhile, some biofilms have been used in moving-bed biofilm reactors (MBBRs) to degrade contaminants in wastewater. Mechanistic understanding of biofilm formation is critical to predict and control biofilm development, yet such understanding is currently incomplete. Here, we reveal the impacts of hydrodynamic conditions and surface roughness on the formation of *Pseudomonas putida* biofilms through a combination of microfluidic experiments, numerical simulations, and fluid mechanics theories. We demonstrate that biofilm growth is suppressed under high flow conditions and characterize the local critical velocity for *P. putida* biofilms to develop, which is about 50 $\mu\text{m/s}$. We further demonstrate that micron-scale surface roughness promotes biofilm formation by increasing the area of low-velocity region. Furthermore, we show that the critical shear stress, above which biofilms cease to form, for biofilms to develop on rough surfaces is 0.9 Pa, over 3 times higher than that for flat surfaces, 0.3 Pa. The results of this study will facilitate future predictions and control of biofilm development on surfaces of drinking water pipelines, blood vessels, sediments, and MBBRs.

12 **ABSTRACT:** The formation of biofilms can increase pathogenic contamination of drinking
13 water, cause biofilm-related diseases, and alter the rate of sediment erosion in rivers and coasts.
14 Meanwhile, some biofilms have been used in moving-bed biofilm reactors (MBBRs) to degrade
15 contaminants in wastewater. Mechanistic understanding of biofilm formation is critical to predict
16 and control biofilm development, yet such understanding is currently incomplete. Here, we
17 reveal the impacts of hydrodynamic conditions and surface roughness on the formation of
18 *Pseudomonas putida* biofilms through a combination of microfluidic experiments, numerical
19 simulations, and fluid mechanics theories. We demonstrate that biofilm growth is suppressed
20 under high flow conditions and characterize the local critical velocity for *P. putida* biofilms to
21 develop, which is about 50 $\mu\text{m/s}$. We further demonstrate that micron-scale surface roughness
22 promotes biofilm formation by increasing the area of low-velocity region. Furthermore, we show
23 that the critical shear stress, above which biofilms cease to form, for biofilms to develop on
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25 study will facilitate future predictions and control of biofilm development on surfaces of
26 drinking water pipelines, blood vessels, sediments, and MBBRs.

27 **INTRODUCTION**

28 Biofilms, consortiums of bacterial cells and extracellular polymeric substances (EPS) attached
29 to surfaces¹, are ubiquitous in rivers²⁻⁴, coastal areas⁵, human organs⁶, and drinking water
30 distribution systems (DWDS)^{7,8}. Many biofilms are harmful because they increase the presence
31 of pathogenic bacteria in DWDS⁹, clog medical devices¹⁰⁻¹², and increase bacterial resistance to
32 bactericides¹³. Many other biofilms, such as those used in moving-bed biofilm reactors
33 (MBBRs)¹⁴, are beneficial as they remove harmful organic compounds and nutrients from waste-
34 water¹⁵. Biofilm thickness is a key parameter to characterize biofilms because it determines when
35 clogging occurs and the efficiency of biofilm-based wastewater treatment plans^{16,17}. The critical
36 condition, above which biofilm thickness becomes zero, is another key parameter because it
37 informs strategies to prevent or control biofilm development. Systematic studies about factors
38 that control biofilm thickness and the critical conditions for biofilm to develop are needed yet
39 currently lacking.

40 Hydrodynamic conditions and surface roughness are two important factors that control biofilm
41 growth¹⁸⁻²⁰, yet their impacts remain controversial. First, some studies show that high flow
42 velocity or shear favors biofilm growth, increases biofilm thickness, and gives rise to a more
43 elastic and resistant biofilm^{21,22}. In contrast, some other studies show that high flow conditions
44 reduce the thickness of biofilms in bioreactors²³. Systematic investigation is needed to reveal the
45 impacts of flow on biofilm development. Second, many studies show that surface roughness
46 increases bacterial adhesion and facilitates biofilm formation²⁴⁻²⁶. In contrast, some other studies
47 show that higher surface roughness reduces bacterial adhesion and biofilm density^{27, 28}.
48 Systematic investigation of biofilm development on rough surfaces with different roughness
49 heights and shapes is also important, because rough surfaces are ubiquitous in natural and

50 artificial environments, e.g., the surfaces of river sediment bed^{29,30}, drinking water pipelines³¹,
51 and MBBRs^{32,33}. Therefore, to prevent harmful biofilms and make use of beneficial biofilms,
52 mechanistic understanding of the combined effects of hydrodynamic conditions and surface
53 roughness on biofilm formation, especially biofilm thickness and the critical conditions to
54 develop biofilms, is needed yet currently remains incomplete.

55 Here we investigate the impacts of hydrodynamic conditions and surface roughness on the
56 formation of *Pseudomonas putida* biofilms. *P. putida* is a bacterium commonly found on the
57 surfaces of aquatic sediment³⁴, terrestrial soils³⁵, and drinking water systems³⁶. In addition, *P.*
58 *putida* has been widely used in bioremediation³⁷ due to its capability to degrade a wide variety of
59 contaminants including lignin^{38,39}, heavy metals^{40,41} and phenols⁴². Fundamental understanding of
60 the factors that control the formation of *P. putida* biofilms is critical for reducing biofilm
61 contamination of our aquatic and terrestrial environments as well as improving the efficiency of
62 biofilm-based bioremediation projects. In this study, we combine biofilm development
63 experiments in custom-designed microfluidic channels with COMSOL simulation and fluid
64 mechanics theories to evaluate the impacts of hydrodynamic conditions and surface roughness on
65 the critical shear stress, above which *P. putida* biofilms cease to form, and the thickness of these
66 biofilms. First, we quantify the impact of flow velocity on biofilm thickness. Second, we
67 quantify the impacts of surface roughness, including its height and shape, on biofilm thickness.
68 Third, we quantify the impacts of surface roughness on the critical shear stress above which
69 biofilms cease to develop. Finally, we discuss the implications of our results in the prediction
70 and control of biofilms in natural aquatic and terrestrial environments, drinking water systems,
71 and biofilm-based reactors used in bioremediation.

72 **MATERIALS AND METHODS**

73 **Bacterial Strains and Culture.** First, we cultured *Pseudomonas putida* KT2442 (a gift from
74 Mohamed Donia's lab, Princeton University) cells from frozen stocks in LB solution overnight
75 (around 16 hours) in an incubator with 200 rpm shaking rate at 30 °C. Second, we transferred the
76 cells in the growth phase to modified M9 solution which has fully characterized chemical
77 composition. Specifically, we centrifuged the 5 mL bacterial cultures in 50 mL tubes at 4,000
78 rpm for 10 minutes, after which, we removed the supernatant (LB) from the tube. Then, the
79 bacteria deposit were diluted by M9 medium solution until the OD₆₀₀ was approximately 0.5. The
80 M9 medium solution was supplemented with micronutrients (0.03 M (NH₄)₆(Mo₇)₂₄, 4 M H₃BO₃,
81 0.3 M CoCl₂, 0.1 M CuSO₄, 0.8 M MnCl₂, 0.1 M ZnSO₄, and 0.1 M FeSO₄) in this study. The
82 carbon source we used here is D-glucose at 1 wt. % concentration.

83

84 **Experimental Platform and Biofilm Development Experiment.** Microfluidic experiments
85 were conducted to characterize development of biofilms on varying surfaces at different flow
86 rates. Schematic diagram of the microfluidic platform is shown in Figure S1. The system consists
87 of a microfluidic chip, a confocal laser scanning microscope (Nikon C2 plus) and a syringe pump
88 (PHD Ultra, Harvard Apparatus). Soft lithography was used to fabricate microfluidic chips. First,
89 we created a mold for the channel on an SU-8-coated silicon wafer using LaserWriter-
90 Heidelberg DWL-200 at the University of Minnesota Nano Center. Afterwards, we created the
91 microfluidics by pouring polydimethylsiloxane (PDMS) with curing agent (Sylgard 184, Dow
92 Corning) onto the molded silicon wafer. After curing the PDMS on a 100 °C hotplate for about
93 one hour, we removed the PDMS from the silicon wafer and punched holes at the channel inlet
94 and outlet with a 1 mm puncher (Med Blades). Then, we bonded the PDMS to a #1.5 cover glass

95 after treating the two bonding surfaces with Asher-Oxygen etcher. The total height of all
96 channels used in this study is 60 μm and the width is 400 μm . The channel measures
97 approximately 5 mm in length from inlet to outlet. During the experiment, the chips were placed
98 on the stage top incubator (UNO-T-H, Okolab) with controlled temperature (30 °C). A syringe
99 pump (PHD Ultra, Harvard Apparatus) is used to precisely control the injection flow rate of the
100 glucose solution. Confocal microscopy was used to image the microfluidic channels and biofilms
101 with 0.31 μm /pixel resolution.

102 Biofilm development experiments were conducted following the steps described below. First,
103 we injected 5 ml *Pseudomonas putida* solution with $\text{OD}_{600} \approx 0.5$ (overnight cultures diluted with
104 M9 solution) into the microfluidics manually with flow rate on the order of mL/min. Afterwards,
105 we switched the three-way valve and injected abiotic M9 solution containing 1 wt. % glucose at
106 different flow rates, from 1 $\mu\text{L}/\text{min}$ to 125 $\mu\text{L}/\text{min}$, to the channel using 3 ml/10 ml/100 ml
107 syringes for 24 hours. As the cells grow and develop biofilms on the side walls of the channel
108 (see Figure S1 for details), we recorded the images of biofilms using a confocal microscope at
109 30-minute intervals. To demonstrate the cells release EPS to form biofilms, we stained the EPS
110 to visualize the biofilms. See the supporting information (SI, Figure S2) for more details.

111

112 **Microfluidic Channel Pattern Design.** To evaluate the impacts of roughness height and
113 geometry on biofilm development, we designed microfluidic channels with three roughness
114 heights and two roughness geometries, round and angular, to represent typical geometries of
115 drinking water pipelines and sediment in natural rivers^{43,44}. The roughness elements were placed
116 at the lower boundary of our microfluidics channel (Figure S1). The upper boundary of our

117 microfluidics channel was kept flat for comparison (Figure S1-b). The relative roughness height
118 δ^* was defined as:

$$119 \quad \delta^* = \frac{h}{R_0} \quad (1)$$

120 Here, $R_0 = 75 \mu\text{m}$ denotes the radius for circular roughness elements and the half height of the
121 equilateral triangle for angular roughness elements (Figure S1-c). h denotes the height of each
122 roughness. For each roughness shape (round and angular), three relative roughness heights $\delta^* =$
123 0.67 ($h_1 = 50 \mu\text{m}$), 1.33 ($h_2 = 100 \mu\text{m}$), and 1.80 ($h_3 = 135 \mu\text{m}$) were considered (Figure S1-d).
124 The central distance between neighboring roughness elements (round and angular) was kept at d
125 $= 100 \mu\text{m}$ (Figure S1-d).

126
127 **Confocal Microscopy.** The development of biofilms on the boundaries of the microfluidic
128 channel were visualized using a Nikon C2+ confocal laser scanning microscope (CLSM) with
129 $0.31 \mu\text{m}$ -horizontal resolution and $0.82 \mu\text{m}$ -vertical resolution. The wavelength of the laser used
130 here is 488 nm . One typical image represents one horizontal scan with 2048 by 2048 pixels, and
131 the biofilms over the channel depth were scanned at 7 vertical positions using the Z-stack
132 function of the Nikon NIS-Elements software. The biofilm cross-sectional images at the middle
133 depth of the channel were used in our analysis. The objective magnification was $10X$ and $20X$.
134 During the experiment, the images were scanned at 30 -minute intervals over 24 hours. At each
135 time step, we imaged biofilms at the inlet, outlet, and middle location of the channel.

136
137 **Image Analysis.** Images obtained from CLSM were saved on a HP-Z4-G4 workstation. To
138 calculate the biofilm thickness on the boundaries, we first converted the confocal images to gray
139 scale images and determined the threshold of color difference between biofilm boundary and

140 water in Image-J (Figure S1-b). Then, we applied this threshold to determine the boundaries of
141 the biofilms after subtracting the biofilm images with the background image (the first image of
142 the time series experiments) using MATLAB. Afterwards, the pixel intensities of the biofilm
143 were summed up and the average biofilm thickness h_B was determined by dividing the total pixel
144 intensities by the length of the field of view.

145
146 **Numerical Simulation.** We simulated the flow in the microfluidic channel in two dimensions
147 using computational fluid dynamics (CFD) finite-element simulation software, COMSOL
148 Multiphysics 5.5 (Burlington, MA, USA). The geometry of the microfluidic channel was set the
149 same as our experimental setup. The Navier-Stokes equation was numerically solved for flow
150 velocity profiles inside the channel using no-slip boundary conditions on all solid surfaces. The
151 stationary simulation was conducted in the fluid phase. Fully developed flow was assumed at the
152 inflow and zero pressure was used at the outflow. Shear stress distribution was calculated based
153 on the velocity profiles. The spatially-averaged shear stress τ_{avg} is defined as the mathematical
154 mean value of the shear stress over the whole channel domain, which was calculated based on
155 the shear stress distribution. The mesh is composed of domain elements ranging in size from
156 61784 to 90788. The mesh area ranges from 1.63 to 2.03 mm². The average quality of an element
157 is around 0.85. More physical parameters used in COMSOL simulation are in the SI (Table S1)

158
159 **Statistical Analysis.** The results of biofilm thickness are shown as mean \pm standard error. The
160 mean value of the biofilm thickness was calculated from the inlet, outlet, and middle part of the
161 microfluidic channel. One biological replicate was conducted at the flow rates of 1 μ L/min, 5
162 μ L/min, 75 μ L/min, and 125 μ L/min for all the roughness types. The error bars indicate standard

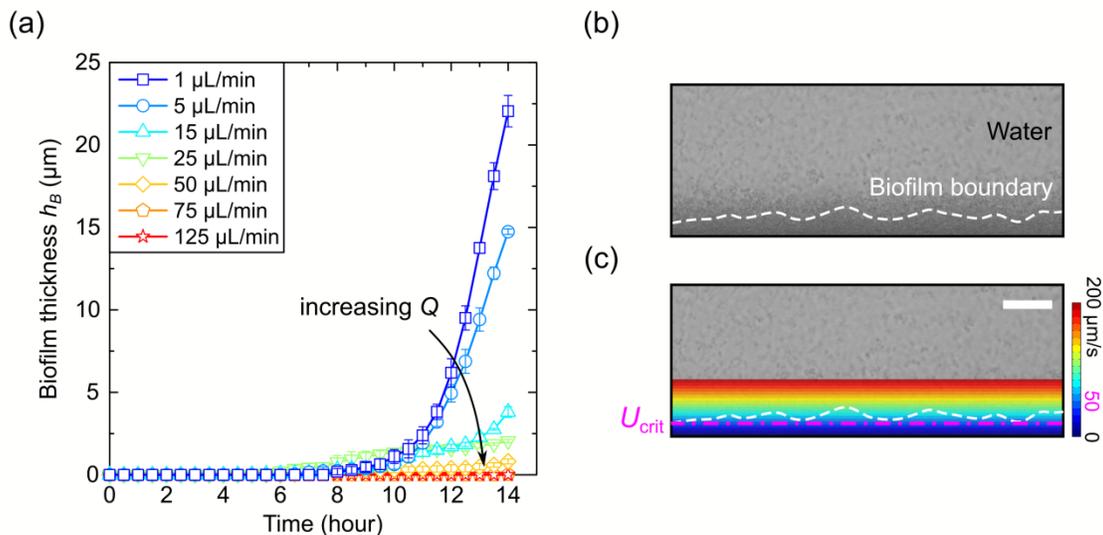
163 error of three measurements. Regression analysis was conducted using MATLAB to predict the
164 critical shear stress under different roughness types and find the confidence level. See the SI
165 (Table S2) for more details.

166 **RESULTS AND DISCUSSION**

167 **Impacts of Hydrodynamic Conditions on Biofilm Thickness.** To reveal the impacts of
168 hydrodynamic conditions on the development of *P. putida* biofilms, we grew *P. putida* cells on
169 the flat surface of custom-built microfluidic channels and measured the thickness of biofilms on
170 the boundary as a function of bacterial growth time (Figure 1). Specifically, we first seed the
171 microfluidic channel with *P. putida* cells by injecting bacterial solution into the microfluidic
172 chamber with flat boundaries. Then, we switched to inject the nutrient solution (M9 medium
173 with 1 wt. % glucose) continuously to allow the cells to grow and biofilms to develop. During
174 the biofilm growth period, we scanned the microfluidic channel using a Confocal Laser Scanning
175 Microscope (CLSM) and measured the average biofilm thickness over time at seven different
176 flow rates (from 1 $\mu\text{L}/\text{min}$ to 125 $\mu\text{L}/\text{min}$) (Figure S3). Our results show that biofilms started to
177 form on the boundaries after 6 to 8 hours of nutrient injection. At low flow rate (e.g., 1 $\mu\text{L}/\text{min}$),
178 biofilm clogging was observed after 14 hours (Figure S4). In the following paragraphs, we
179 discuss the impacts of flow on biofilm development before 14-hour growth time.

180 First, we demonstrate the impacts of flow rate on the thickness of biofilms developed on the
181 flat boundary. At the low flow rate range (1 $\mu\text{L}/\text{min}$ to 5 $\mu\text{L}/\text{min}$), we observed rapid increase in
182 biofilm thickness over the 14-hour growth time (Figure 1-a). The biofilm thickness increased
183 exponentially from 8 to 14 hours, indicating that biofilm development is contributed by
184 exponential increase of cell density during the growth phase¹¹ (Figure S5). At middle flow rate
185 range (15 $\mu\text{L}/\text{min}$ to 25 $\mu\text{L}/\text{min}$), the biofilm thickness did not increase exponentially over time
186 and was smaller than the thickness of those grown under the low flow rate range. At the high
187 flow rate range (50 $\mu\text{L}/\text{min}$ to 125 $\mu\text{L}/\text{min}$), no biofilm was observed at the boundary, namely
188 biofilm ceased to develop at high flow (>50 $\mu\text{L}/\text{min}$). The prevention of biofilm development by

189 high flow is likely because bacterial cells can be swept away by flow and detach from surfaces
 190 when the flow velocity or shear stress is higher than a critical value.



191
 192 **Figure 1.** (a) The thickness of *P. putida* biofilms developed on the flat surface of a microfluidic
 193 channel (shown in (b)) as a function of time. (b) Confocal microscopic image of biofilms (dark
 194 gray color) developed on the flat surface of the microfluidic channel. The white dashed curve
 195 denotes the boundary of the biofilm accumulation region identified based on contrast of pixel
 196 intensity. The flow rate is $Q = 1 \mu\text{L}/\text{min}$. (c) Flow velocity distribution in color superimposed on
 197 gray-scale confocal image shown in (b). The pink dot-dashed line denotes the line with velocity
 198 equal to $50 \mu\text{m}/\text{s}$, which is the local critical velocity for biofilm to develop U_{crit} . The scale bar is
 199 $25 \mu\text{m}$.

200
 201 Second, we quantify the local critical conditions for *P. putida* biofilms to develop, by
 202 combining the experimental results with numerical simulation of the flow field in the
 203 microfluidic channel using COMSOL (Figure 1-b, c). By comparing the CLSM images of
 204 biofilms with the flow field simulation, we found that biofilms (with boundary indicated by the

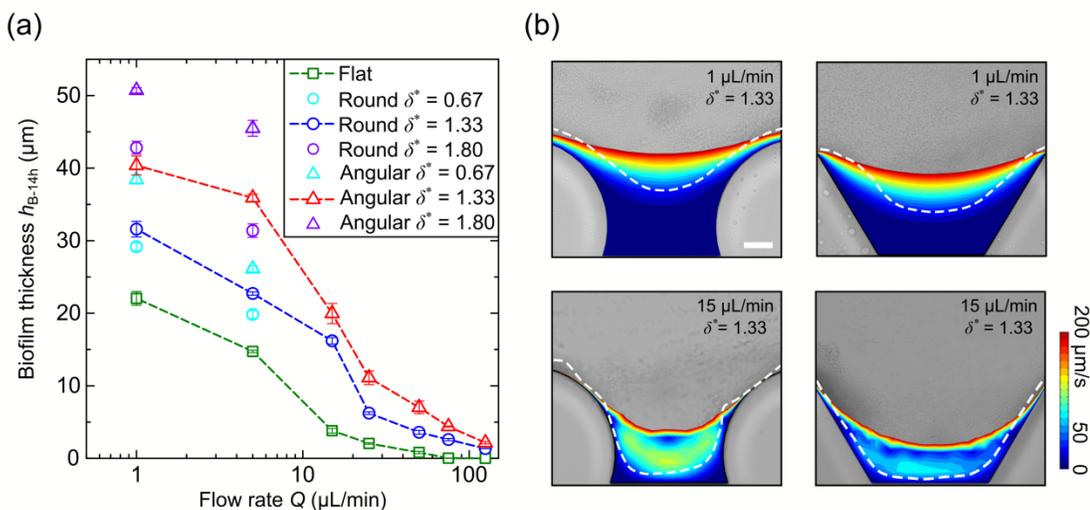
205 white dashed lines in Figure 1-b, c) accumulated at regions with flow velocity lower than 50
206 $\mu\text{m/s}$ (the pink lines in Fig. 1-c), suggesting that the local critical velocity for the *P. putida*
207 biofilms to develop is around $U_{\text{crit}} = 50 \mu\text{m/s}$. Furthermore, we conducted the same analysis for
208 channels with varying roughness types at different flow rates (Figure 2-b) and found that $U_{\text{crit}} =$
209 $50 \mu\text{m/s}$ regardless of flow rates and surface roughness. This indicates that the local critical
210 velocity for *P. putida* biofilms to develop is always $50 \mu\text{m/s}$ and not affected by boundary
211 roughness. We caution that U_{crit} may be different for different bacterial strains due to the
212 difference in growth rates and bacterial biofilm cohesion abilities.

213

214 **Impacts of Roughness Heights on Biofilm Thickness.** Next, we evaluate the impact of
215 surface roughness on biofilm growth by comparing the development of biofilms on surfaces of
216 varying roughness in microfluidic channels (Figure S3 and S6). Specifically, we measured the
217 time evolution of the average thickness of biofilms developed on flat surfaces and surfaces with
218 round and angular roughness elements of varying heights (Figure 2-a). The average biofilm
219 thickness was defined as the effective thickness assuming a flat surface, i.e., equal to the area of
220 biofilm in 2D divided by the straight-line length of the boundary. As shown in Figure 2-a,
221 biofilms developed on rough surfaces have larger average thickness than those developed on flat
222 surfaces. Furthermore, for the same roughness shape (round or triangular), the average biofilm
223 thickness increases with increasing relative roughness height δ^* . The increase in average biofilm
224 thickness with increasing roughness height is likely caused by the increase in the area of low
225 flow velocity regions induced by the roughness. Above a flat surface, the streamline is parallel to
226 the boundary (Figure 1-c), such that the region with velocity smaller than U_{crit} , the local critical
227 velocity for biofilm to develop, is a thin rectangular region near the flat surface. In comparison,

228 in channels with rough surfaces, the region with velocity smaller than U_{crit} include the sheltered
 229 regions between the roughness elements, which allow more bacterial cells to attach to the surface
 230 and form biofilms (Figure 2-b).

231 In short, we demonstrated that micro-scale surface roughness promotes biofilm formation, i.e.,
 232 increases average biofilm thickness, by increasing the area of low-velocity region which
 233 provides shelter for the bacteria to form biofilms. We caution that the effect of nanoscale
 234 roughness may be different because some studies showed higher nanoscale surface roughness
 235 reduce bacterial adhesion and inhibit biofilm formation^{27,28}.



236
 237 **Figure 2.** (a) The average thickness of *P. putida* biofilms developed on flat and rough surfaces
 238 with round and angular elements at varying flow rates. The symbols and error bars represent the
 239 mean value and standard error of the biofilm thickness obtained from four replicate
 240 measurements/experiments respectively. (b) Images of flow velocity in color superimposed on
 241 gray-scale confocal images of biofilms on surfaces with varying roughness at varying flow
 242 velocity: (from left to right) relative roughness height $\delta^* = 1.33$, flow rate $Q = 1 \mu\text{L}/\text{min}$, round
 243 shape; $\delta^* = 1.33$, $Q = 1 \mu\text{L}/\text{min}$, angular shape; $\delta^* = 1.33$, $Q = 15 \mu\text{L}/\text{min}$, round shape; $\delta^* =$

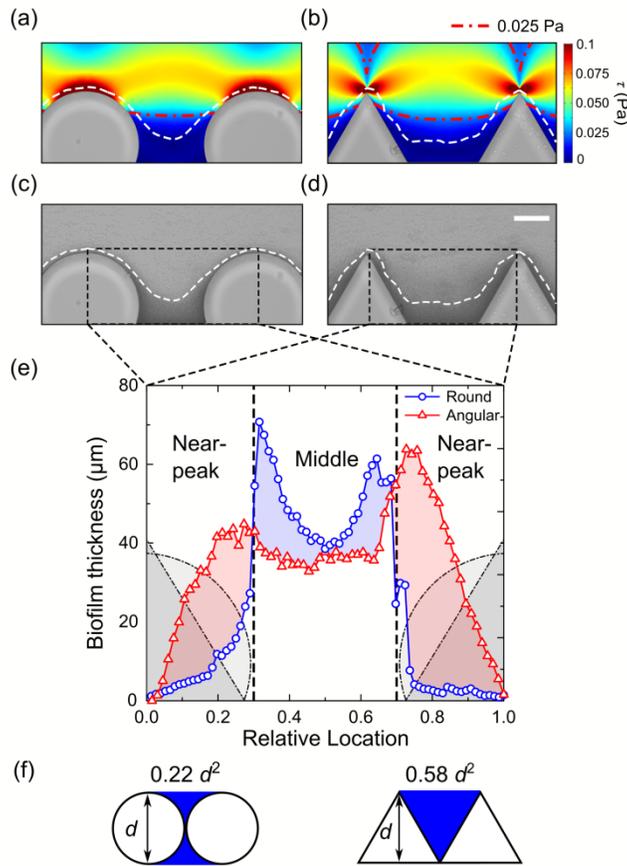
244 1.33, $Q = 15 \mu\text{L}/\text{min}$, angular shape. The white dashed lines denote the boundary of biofilms
245 identified based on contrast of pixel intensity. The scale bar is $25 \mu\text{m}$.

246

247 **Impacts of Roughness Shapes on Biofilm Thickness.** Furthermore, we evaluate the impacts
248 of roughness shape on biofilm development. For the same relative roughness height δ^* , the
249 average thickness of biofilms developed on surfaces with angular roughness elements is
250 consistently larger, by up to about 2 times than that for surfaces with round roughness (Figure 2-
251 a), suggesting that surfaces with angular roughness can further promote biofilm formation
252 compared with round shape.

253 To demonstrate how roughness shape impacts biofilm development, we simulated the shear
254 stress distribution in channels with the round and angular roughness using COMSOL (Figure 3-a,
255 b). In channels with angular roughness element, the higher shear stress region (shear stress $>$
256 0.025 Pa , indicated by the red dot-dashed line in Figure 3-a, b) only exists at the peak of the
257 angular roughness element. In contrast, in channels with round roughness, the higher shear stress
258 region extends from the peak location to the middle region of two adjacent cylinders. In the
259 middle region between two adjacent roughness elements (relative location between 0.3 and 0.7),
260 the amount of biofilm accumulation in channel with round roughness is 1.3 times larger than that
261 in the channel with angular roughness (Figure 3-e). However, outside the middle region, or in the
262 “near-peak” regions, the amount of biofilm accumulated in channel with angular roughness is 4.7
263 times larger than that in channel with round roughness, which is why overall there are 60% more
264 biofilms developed on the surface with angular roughness than on the surface with round
265 roughness. The more abundant biofilms in channels with angular roughness can also be
266 explained by the geometry itself, because the area of the sheltered region between tightly-packed

267 angular roughness is 2.6 times the area between round roughness (dark blue color in Figure 3-f).
 268 Larger sheltered areas have been anticipated to promote biofilm development by increasing the
 269 nutrient circulation and mass transport⁴⁵. In short, we found that channels with angular roughness
 270 have larger biofilm thickness due to larger areas of low shear stress region between roughness
 271 elements, which provide more shelter for bacteria to form biofilm.



272
 273 **Figure 3.** Simulated shear stress distribution (a and b) in color superimposed on gray-scale
 274 confocal images (c and d) of biofilms in microfluidic channels with round and angular roughness
 275 elements ($\delta^* = 1.33$, $Q = 5 \mu\text{L}/\text{min}$). The white dashed curve denotes the boundary of the biofilm.
 276 The red dot-dashed line shows the contour of $\tau = 0.025$ Pa based on the simulation. The scale bar
 277 is $50 \mu\text{m}$. (e) The distribution of the biofilm thickness between the centers of neighboring
 278 roughness elements in the dashed boxes region shown in (c) and (d). The light blue area shows

279 the difference in the amount of biofilm accumulation in the middle part of the channel (relative
280 location between 0.3 and 0.7, the black dashed lines indicate the boundary between “near-peak”
281 region and middle part) between the surface with round and angular roughness. The light red
282 area shows the difference in the amount of biofilm accumulation in the “near-peak” region. The
283 grey areas show the contour of the round and angular roughness shapes. (f) Schematic diagrams
284 of the sheltered region (dark blue color) between tightly-packed round and angular roughness
285 elements.

286

287 **Impacts of Roughness on Critical Conditions of Biofilm Development.** Finally, we reveal
288 the impacts of roughness on the spatially-averaged critical shear stress τ_{crit} , above which biofilms
289 cease to develop.

290 First, we combine theories and simulation to calculate τ_{crit} for biofilms to develop on a flat
291 surface from U_{crit} , which is the local critical velocity for biofilms to develop and equals to 50
292 $\mu\text{m/s}$ for *P. putida*. For the experiments in which bacterial solution was injected into the
293 microfluidic channel with width D and flat boundaries at flow rate Q , the Reynolds number
294 ($\text{Re} = \frac{\rho U D_h}{\mu}$, ρ is the density of water, U is the velocity at the inlet, D_h is the hydraulic diameter,

295 μ is the dynamic viscosity of water) is at the range of 0.09 to 11.3, thus the flow is laminar.

296 Assuming a fully developed flow, the velocity profile in the channel can be described by Hagen-
297 Poiseuille flow, i.e., with parabolic distribution^{46, 47}:

$$298 \quad U = \frac{3Q[1 - (2y/D)^2]}{2A} \quad (2)$$

299 where $A = 0.024 \text{ mm}^2$ is the cross-section area of the channel.

300 Consider biofilms only develop in regions with velocity less than U_{crit} (Figure 1-c), then the
 301 thickness of biofilms, h_B , on the flat boundary can be estimated by substituting U_{crit} into equation
 302 (2):

$$303 \quad h_B = \frac{D}{2} - \frac{D}{2} \sqrt{1 - \frac{2U_{crit}A}{3Q}} \quad (3)$$

304 We assume that no biofilm will develop on the flat surface when the thickness of this low
 305 velocity biofilm zone h_B is less than 1/5 of the bacterial body length, which is 0.1 μm for *P.*
 306 *putida*⁴⁸. Substitute $h_B = h_{crit} = 0.1 \mu\text{m}$ into equation (3), we found the critical flow rate Q_{crit} for *P.*
 307 *putida* biofilms to develop is:

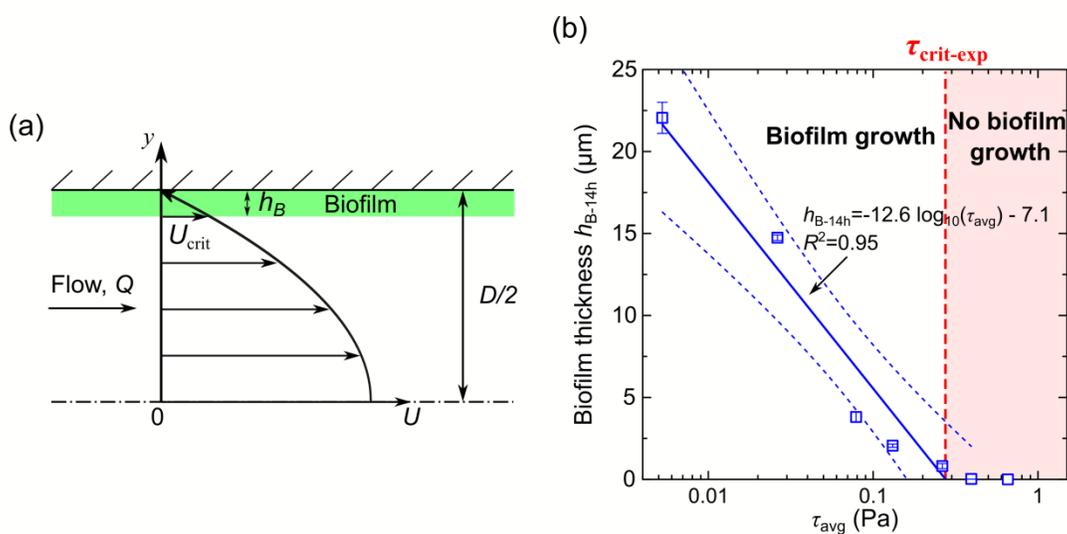
$$308 \quad Q_{crit} = \frac{2U_{crit}A}{3[1 - (1 - 2h_{crit}/D)^2]} \quad (4)$$

309 Therefore, based on the parabolic velocity distribution (Equation 2), the critical shear stress τ_{crit}
 310 to develop biofilms is:

$$311 \quad \tau_{crit-theo} = \mu \left. \frac{dU}{dy} \right|_{y=D/2} = \frac{6\mu Q_{crit}}{AD} \quad (5)$$

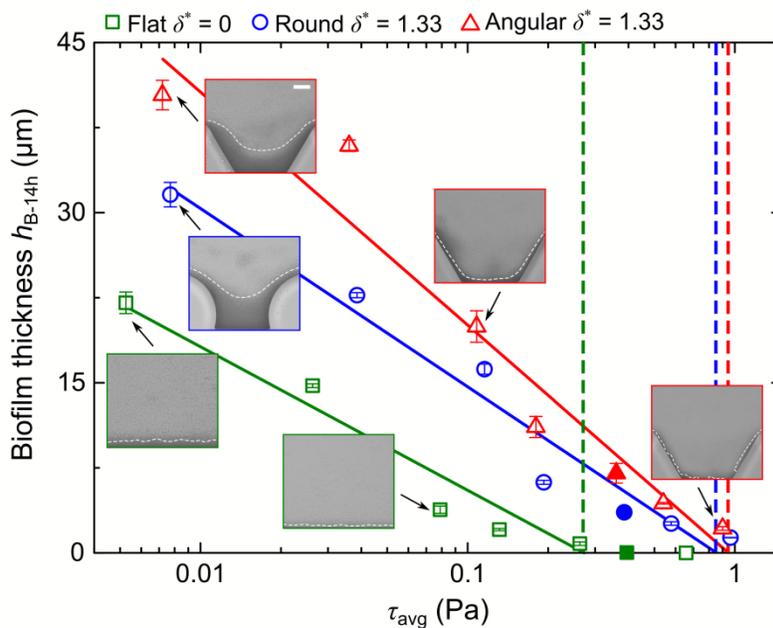
312 By using equation (5), we predict that the theoretical critical shear stress for *P. putida* biofilms
 313 to develop is $\tau_{crit-theo} = 0.4 \text{ Pa}$. To test the validity of our critical shear stress theory (Equations 2-
 314 5), we compared the predicted critical shear stress $\tau_{crit-theo} = 0.4 \text{ Pa}$ with the critical stress
 315 estimated from our measurements. Specifically, we plotted the average biofilm thickness at 14-
 316 hour growth-time, h_{B-14h} , measured from confocal images, versus the shear stress τ_{avg} calculated
 317 from the CFD simulation results (Figure 4-b). Our results show that h_{B-14h} and τ_{avg} are linearly
 318 dependent and above a certain critical shear stress, no biofilms were observed on the surface. To
 319 estimate this critical shear stress, we fitted a linear line (blue line in Figure 4-b) to the h_{B-14h}
 320 versus τ_{avg} data and found that the x-intercept, which represents the critical shear stress $\tau_{crit-exp}$,

321 and is 0.3 Pa for the flat surface. The agreement between $\tau_{\text{crit-exp}} = 0.3$ Pa based on measurements
 322 and the $\tau_{\text{crit-theo}} = 0.4$ Pa based on theoretical calculation confirms our hypothesis that the critical
 323 conditions to develop biofilms is controlled by local flow velocity. Our predicted and measured
 324 τ_{crit} is also consistent with a previous study, which shows that the critical shear stress for
 325 microalgae *Chlorella vulgaris* biofilms to develop on the surface of flat-panel photobioreactor is
 326 0.2 Pa⁴⁹.



327
 328 **Figure 4.** (a) Schematic diagram of the theoretical parabolic velocity distribution (black curve,
 329 Equation 2) in the microfluidic channel with flat surfaces. U_{crit} denotes the local critical velocity
 330 for biofilms to develop and h_B denotes the biofilm thickness. The light green color represents the
 331 region where bacterial biofilms accumulate. (b) The biofilm thickness h_{B-14h} measured from
 332 confocal images (after 14-hour growth period) as a function of the shear stress τ_{avg} calculated
 333 from CFD simulation. The red dashed line indicates the critical shear stress τ_{crit} , above which
 334 biofilms do not develop on the flat surface. The solid blue line indicates the linear fit $h_{B-14h} = -$
 335 $12.6 \log_{10}(\tau_{\text{avg}}) - 7.1$. The blue dashed line represents the 90 % confidence interval.
 336

337 Furthermore, we demonstrate the impact of surface roughness on τ_{crit} . We plotted the average
 338 biofilm thickness as a function of the average shear stress (Figure 5) and identified τ_{crit} for each
 339 rough surface. Compared with the flat surfaces for which the measured $\tau_{\text{crit-flat}} = 0.3$ Pa, the τ_{crit}
 340 for biofilms to develop on surfaces with round roughness with $\delta^* = 1.33$ is 0.8 Pa, and on
 341 surfaces with angular roughness with $\delta^* = 1.33$ is 0.9 Pa. Therefore, the critical shear stress τ_{crit}
 342 for biofilms to develop on surfaces with angular and round roughness is about 3 times as large as
 343 that for flat surfaces. Our results highlight the important role of surface roughness on biofilm
 344 development.

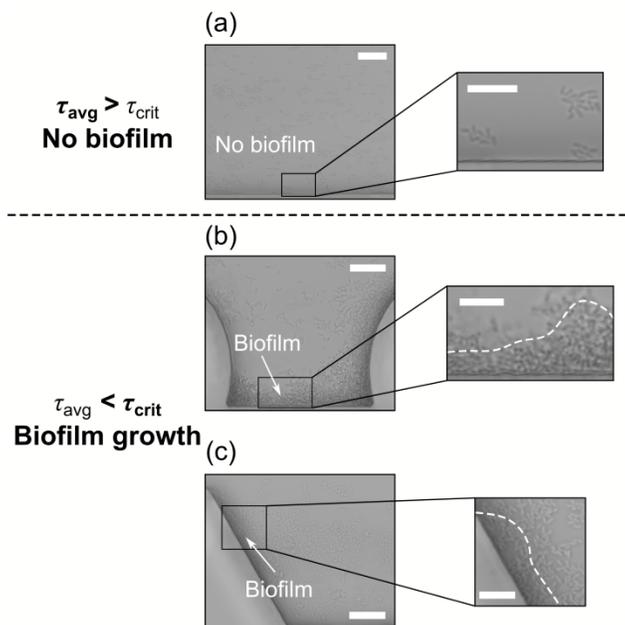


345
 346 **Figure 5.** Measured biofilm thickness after 14-hour growth period as a function of shear stress
 347 τ_{avg} for flat surface (green) and rough surfaces with round elements (blue) and angular elements
 348 (red). The dashed vertical lines indicate the critical shear stress for the flat surface $\tau_{\text{crit-flat}}$ (green),
 349 and surfaces with round roughness $\tau_{\text{crit-round}}$ (blue) and angular roughness $\tau_{\text{crit-angular}}$ (red). The three
 350 symbols filled with color represent the data ($\tau_{\text{avg}} = 0.38 \pm 0.02$ Pa) used for Figure 6. The insets

351 show confocal images for representative cases indicated by the black arrows. The scale bar is 25
352 μm for both insets.

353

354 At about the same shear stress conditions, e.g., $\tau_{\text{avg}} = 0.38 \pm 0.02 \text{ Pa}$, we anticipate that no
355 biofilm would developed on the flat surface, because the τ_{avg} is larger than $\tau_{\text{crit-flat}} = 0.3 \text{ Pa}$ (Figure
356 6). In contrast at the same shear stress $\tau_{\text{avg}} = 0.38 \pm 0.02 \text{ Pa}$, we predict that biofilms would
357 develop on the rough surfaces with both angular and round roughness elements, because the τ_{avg}
358 is smaller than $\tau_{\text{crit-rough}} = 0.8\text{-}0.9 \text{ Pa}$. Our predictions are confirmed by our microfluidic
359 observations of biofilms developed on flat and rough surfaces under similar average shear stress
360 ($\tau_{\text{avg}} = 0.38 \pm 0.02 \text{ Pa}$), as shown in Fig. 6, suggesting that surface roughness indeed increases τ_{crit} ,
361 making it more difficult to prevent biofilm growth on rough surfaces by increasing flow velocity.
362 Additionally, our results suggest that a higher shear stress or flow rate is required to prevent
363 biofilm formation on rough surfaces, such as rough surfaces of angular sediment deposits in
364 fluvial system², drinking water pipes⁷, and MBBRs used in wastewater treatment plants³³.



365

366 **Figure 6.** The development of biofilms on flat and rough surfaces under similar average shear
367 stress ($\tau_{\text{avg}} = 0.38 \pm 0.02$ Pa). (a) On the flat surface, no biofilm developed on the boundary
368 because the shear stress in the channel τ_{avg} is larger than the critical shear stress $\tau_{\text{crit-flat}} = 0.3$ Pa.
369 On surfaces with round roughness (b) and angular roughness (c) with similar shear stress,
370 biofilms can develop on surfaces, as the shear stress τ_{avg} is smaller than the critical shear stress
371 $\tau_{\text{crit-rough}} = 0.8-0.9$ Pa. The white dashed lines denote the boundary of biofilms. The scale bar is 25
372 μm . The scale bar of zoom-in images is 10 μm .

373

374 In conclusion, we demonstrate the impacts of hydrodynamic conditions and surface roughness
375 on the thickness of and the critical conditions to develop *P. putida* biofilms through
376 systematically-controlled microfluidic experiments and CFD simulations. First, we show that
377 biofilm growth is suppressed under high flow velocity. By combining experimental and
378 simulation results, we demonstrate that the local critical velocity for *P. putida* biofilms to
379 develop is 50 $\mu\text{m/s}$, and this critical value is the same for the range of flow rates (1 $\mu\text{L/min}$ -125
380 $\mu\text{L/min}$) and roughness considered here. Furthermore, we propose a theoretical model to predict
381 the critical shear stress, above which biofilms ceases to develop on flat surfaces, which is $\tau_{\text{crit-flat}} =$
382 0.3 Pa. In addition, we revealed the impacts of roughness, including its height and shape, on the
383 biofilm formation. We show that roughness elements create sheltered low flow regions that
384 promote biofilm formation. Compared with round roughness elements, angular roughness
385 elements provide larger area of low flow region, which further facilitate biofilm accumulation.
386 Finally, we demonstrate that the critical shear stress for biofilm to develop on rough surfaces
387 with angular and round roughness is 0.9 Pa and 0.8 Pa, respectively, which are about 3 times
388 higher than that on flat surfaces (0.3 Pa).

389 Our study highlights the important role of hydrodynamic conditions and surface roughness in
390 controlling biofilm formation on surfaces and provides systematic and quantitative
391 characterization of these effects. While our work only considers the initial stages of the biofilm
392 formation process and a single-species biofilm, we expect that the experimental method and
393 predictive equation developed in this study can be extended to study multi-species biofilms in the
394 future. The bacterium used here, *Pseudomonas putida*, is a common soil bacterium and a widely-
395 used strain in bioremediation. Therefore, the results presented here have important implications
396 in predicting and controlling biofilm-related contaminants in aquatic and terrestrial environments
397 as well as in bioremediation industries. Specifically, our results can be used to determine the
398 optimal flow rates to mitigate biofouling in drinking water distribution systems, predict the
399 existence and thickness of biofilms on aquatic sediment and terrestrial soil, as well as facilitate
400 selection of surface roughness and flow velocity to control the thickness of biofilms in MBBRs
401 to optimize bioremediation efficiency.

402 AUTHOR INFORMATION

403

404 **Corresponding Author**

405 *Judy Q. Yang (judyyang@umn.edu)

406

407 **Author Contributions**

408 G.W. and J.Q.Y. conceived and designed the project. G.W. and J.Q.Y. designed the experiments.

409 G.W. conducted the experiments. G.W. and J.Q.Y. analyzed the data and wrote the paper.

410

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413

414 **Notes**

415 The authors declare no competing financial interest.

416

417 **Data Availability Statements**

418 Data will be made available in the Data Repository for University of Minnesota repository

419 (<https://doi.org/10.13020/afnk-kp31>).

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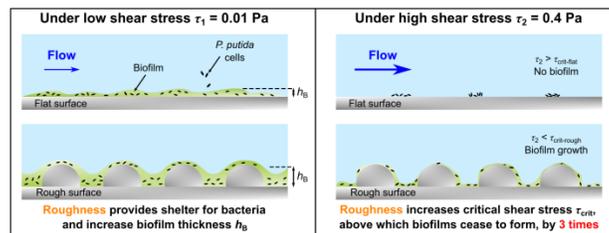
421 **Acknowledgment**

422 We thank Dr. J Sanfilippo for help with the strains. Portions of this work were conducted in
423 the Minnesota Nano Center, which is supported by the National Science Foundation through the
424 National Nanotechnology Coordinated Infrastructure (NNCI) under Award Number ECCS-
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426

427 Briefs

428 Abstract Graphic:



429

430

431 Synopsis

432 This study demonstrates that microscale surface roughness can increase the critical shear stress
433 to form biofilms by 3 times.

434

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Supporting Information

Impacts of hydrodynamic conditions and surface roughness on the critical condition to develop and thickness of *Pseudomonas putida* biofilms

Guanju Wei^{1,2}, *Judy Q. Yang*^{1,2*}

¹Saint Anthony Falls Laboratory, University of Minnesota, Minneapolis MN, USA; ²Department of Civil, Environmental, and Geo-Engineering

Corresponding Author:

*Judy Q. Yang (judyyang@umn.edu)

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Figure S4. Biofilms in microfluidic channels continue growing after 14 hours and start to clog the channel after 24 hours.

Figure S5. The biofilm growth follows exponential law under low flow rates: 1 $\mu\text{L}/\text{min}$ (a) and 5 $\mu\text{L}/\text{min}$ (b).

Figure S6. Cross-sectional images of the biofilms at 14-hour growth time in channels with flat boundaries and boundaries with round and angular roughness at two different flow rates and three roughness heights.

Tables

Table S1. Parameters used in COMSOL simulation.

Table S2. The 90% confidence interval of critical shear stress τ_{crit} , p value, and R2 were calculated by regression analysis using MATLAB.

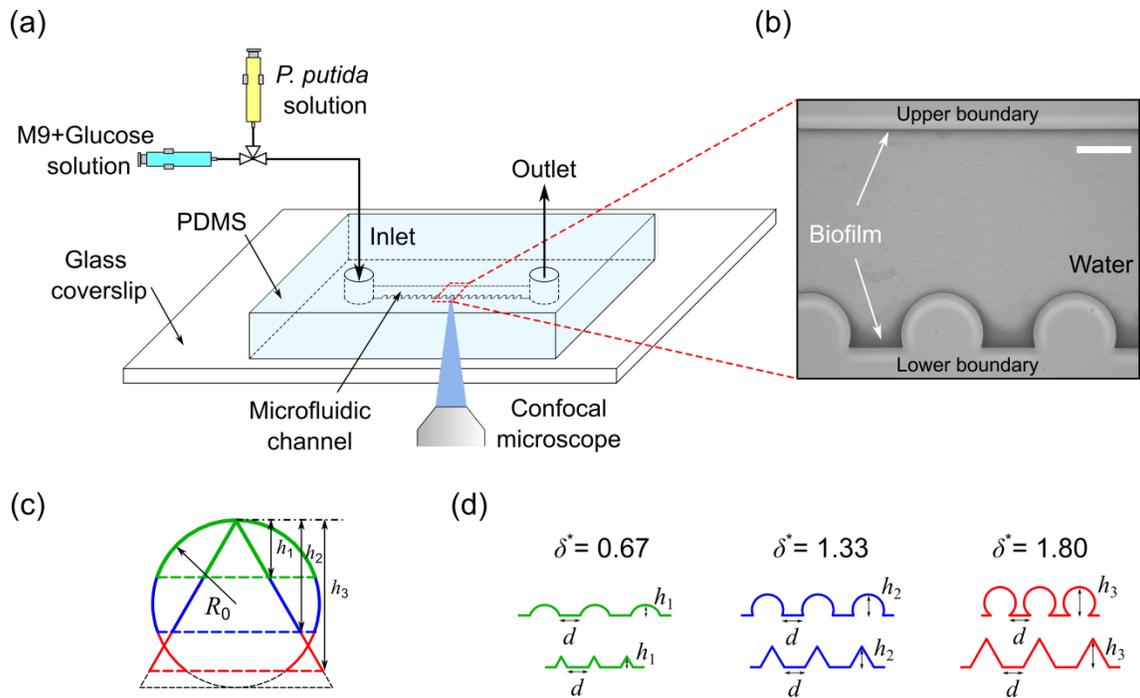


Figure S1. (a) Schematic diagram of the experimental set up. (b) Cross-sectional image of the microfluidic channel. Biofilms (gray color) accumulate at the upper and lower boundaries of the channel. The scale bar is 100 μm . (c) The relative roughness height δ^* is defined as h/R_0 . $R_0 = 75$ μm denotes the radius of the circle and half of the triangle height. h denotes the height of each roughness on the surface: $h_1 = 50$ μm , $h_2 = 100$ μm , $h_3 = 135$ μm . (d) Six types of rough surfaces were used in this study with three relative heights ($\delta^* = 0.67, 1.33, 1.80$) and two types of roughness shape (round and angular) at the lower boundary. The distance between the neighboring roughness elements for all cases is the same, i.e., $d = 100$ μm .

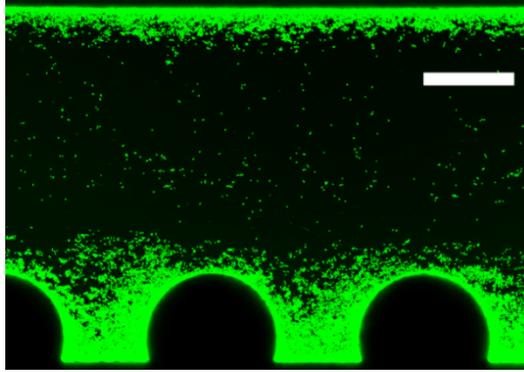


Figure S2. Confocal image of the biofilm stained with EPS dyes after the 14-hour experiments at flow rate of 5 $\mu\text{L}/\text{min}$, $\delta^* = 1.33$. EPS is visualized with green fluorescent dyes¹. The EPS stains included 5 μM of SYTO-9 green fluorescent nucleic acid stain (Thermo Fisher Scientific, USA), 20 $\mu\text{g}/\text{mL}$ fluorescein isothiocyanate (FITC) conjugated Concanavalin A from *Canavalia ensiformis* (Sigma), and 20 $\mu\text{g}/\text{mL}$ FITC conjugated lectin from *Triticum vulgaris* (Sigma). The scale bar is 100 μm .

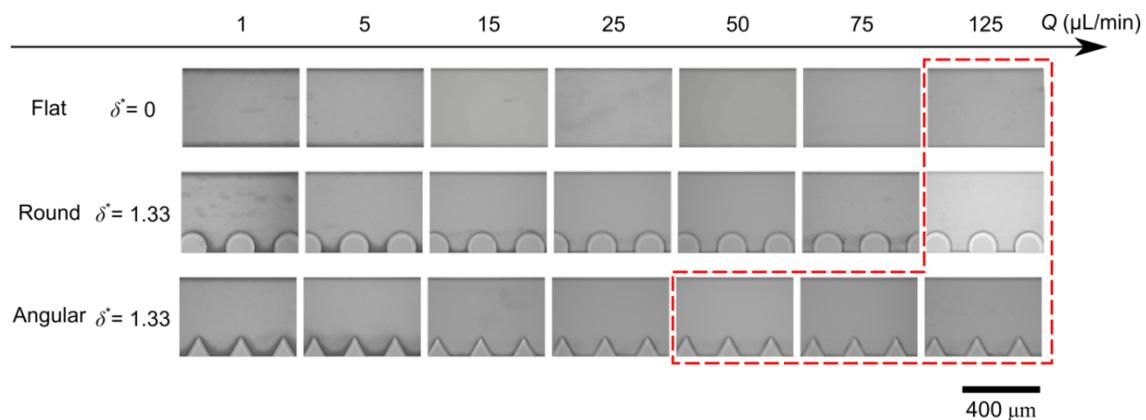


Figure S3. Cross-sectional images of the biofilms at 14-hour growth time in channels with flat boundaries and boundaries with round and angular roughness (both with roughness relative height $\delta^* = 1.33$) at seven flow rates. Red dashed line represents cases with no biofilm growth.

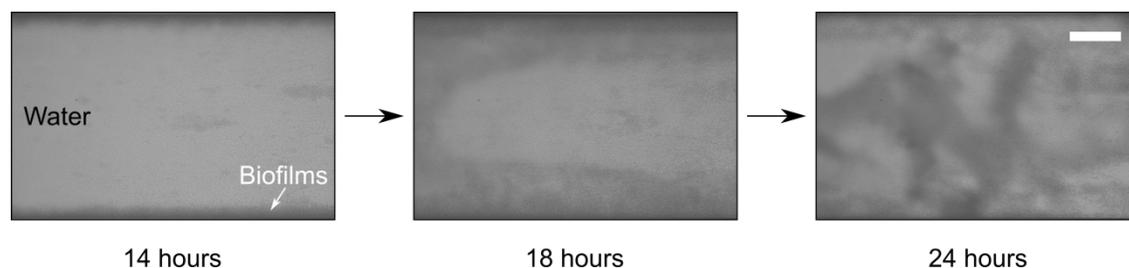


Figure S4. At low-flow conditions ($<5 \mu\text{L}/\text{min}$), biofilms in microfluidic channels continue growing after 14 hours and start to clog the channel after 24 hours. The scale bar is 100 μm .

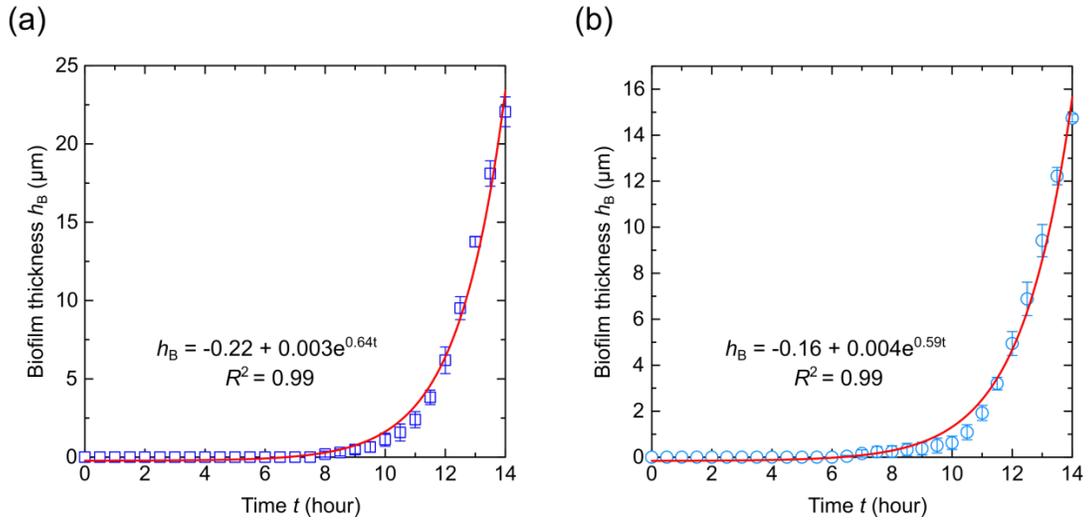


Figure S5. The biofilm growth follows exponential law under low flow rates: $1 \mu\text{L}/\text{min}$ (a) and $5 \mu\text{L}/\text{min}$ (b).

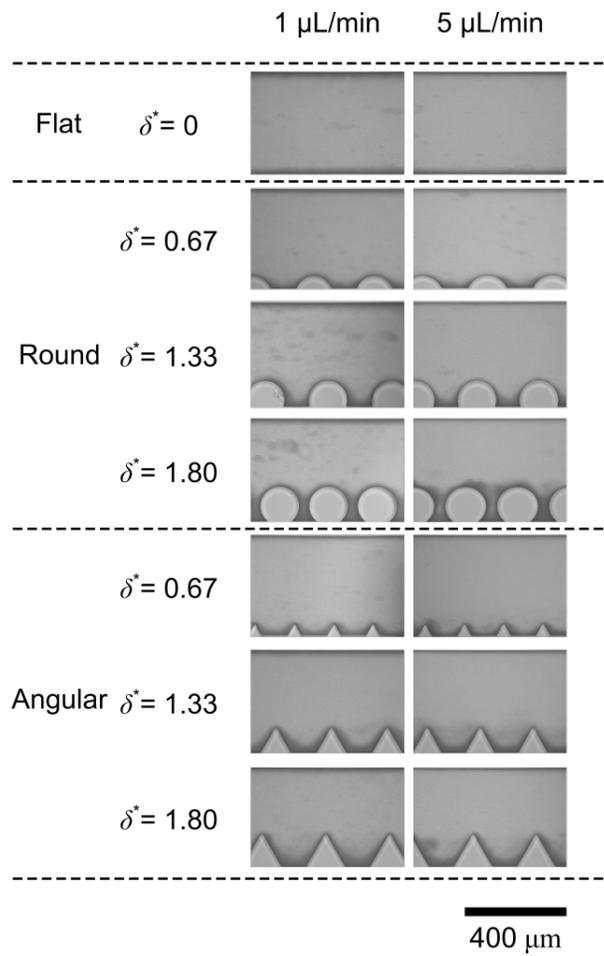


Figure S6. Cross-sectional images of the biofilms at 14-hour growth time in channels with flat boundaries and boundaries with round and angular roughness at two different flow rates and three roughness heights.

Table S1. Parameters used in COMSOL simulation.

Flow conditions	Laminar flow
	Incompressible flow
Density	995.6 kg/m ³
Dynamic viscosity	0.001 Pa·s
Average inflow velocity	0.09 m/s
	0.05 m/s
	0.03 m/s
	0.02 m/s
	0.01 m/s
	0.003 m/s
	0.0007 m/s
Temperature	303.15 K

Table S2. The 90% confidence interval of critical shear stress τ_{crit} , p value, and R^2 were calculated by regression analysis using MATLAB.

	90% confidence interval	p	R^2
Flat	0.19 ~ 0.48	1.0×10^{-3}	0.95
Round	0.59 ~ 1.44	1.1×10^{-4}	0.96
Angular	0.61 ~ 1.84	2.2×10^{-4}	0.95

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(1) Drescher, K.; Shen, Y.; Bassler, B.L.; Stone, H.A. Biofilm streamers cause catastrophic disruption of flow with consequences for environmental and medical systems. *Proceedings of the National Academy of Sciences*. 2013, *110*(11), 4345-4350.